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# 1 Title: Structured variability of steady-speed locomotion in rats 2 3 André Schmidt<sup>1\*</sup>, Audrone R. Biknevicius<sup>1</sup> 4 **Authors**: 5 <sup>1</sup>Department of Biomedical Sciences 6 7 Heritage College of Osteopathic Medicine 8 Department of Biomedical Sciences Ohio University, Athens, 45701, USA 9 \*e-Mail: schmidta@ohio.edu 10 11 12

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## **SUMMARY**

By examining key locomotor parameters during terrestrial locomotion on a substrate without irregularities, we show that rats frequently accelerate and decelerate between two consecutive steps while maintaining an *overall* steady-speed and that the touchdown order of contralateral limbs significantly influences those speed adjustments. The latter highly correlates with significant adjustments in relative forelimb protraction at touchdown and hindlimb extension at lift off. We conclude that this remarkable level of variability in limb coordination would clearly be advantageous for the functional flexibility needed during terrestrial locomotion on much more irregular (rough) natural terrain. In addition, its occurrence on a substrate lacking irregularities suggests that much of stable, terrestrial steady-speed locomotion in rats is mechanically controlled.

Key words: rat; locomotion; stability; inter-step variation

#### INTRODUCTION

Terrestrial gaits are rhythmic patterns of footfalls. Because these cyclical movements commonly occur at high frequencies (i. e., during running, it is widely accepted that they cannot be actively controlled only by the nervous system (e.g., Biewener and Daley, 2007; Blickhan et al., 2010; Hooper, 2012). During perturbed locomotion, animals rather rely on passive dynamic mechanisms that include spring-mass mechanics and intrinsic mechanisms (see also Biewener and Daley, 2007). In humans and birds, simple spring-mass mechanics mitigate to sudden changes in terrain height (Daley and Biewener, 2006; Geyer et al., 2005; Grimmer et al., 2008; Seyfarth et al., 2008). Limbs acts as springs and help the system to return to locomotor trajectory in between a single-step. Interestingly, bipeds maintain passive spring-mass dynamics when limb contact angle, effective limb length and limb stiffness exhibit particular limited ranges (Seyfarth et al., 2002; Geyer et al., 2005; Grimmer et al., 2008). In addition, intrinsic mechanisms, including force-length, force-velocity and history-dependent properties as well as postural effects on joint dynamics at the musculoskeletal level help to reduce the control effort and consequently the complexity of the nervous system (see also Biewener and Daley, 2007).

However, that does not suggest that neural control is not required during perturbed locomotion. Indeed, active neural control and passive mechanisms are linked. An animal that predicts a perturbation, for example, changes limb posture (e.g., contact angle) *via* muscle activity (Grimmer et al., 2008). Even with a short delay, reflex feedback may also contribute to further stabilization within a single stance phase (e.g., Hiebert and Pearson, 1999). Importantly, control mechanisms greatly depend on locomotor speed and body size (e.g., Biewener and Daley, 2007; Hooper, 2012). During fast locomotion such as running, mechanical control mechanisms likely play a predominant role for locomotor stability due to neural transmission delays that could be destabilizing (e.g., Full and Koditschek, 1999; Full et al., 2002; Biewener and Daley, 2007). Walking gaits, which occur at slower speeds, are rather likely to be more actively than passively controlled. In addition, body size plays a crucial role in terms of neural feedback (Hooper, 2012). Mice, for example, have much shorter times for corrective neural computations than horses (Hooper, 2012).

However, gait mechanics are not perfectly reproduced between steps, leading to some level of variation even under restricted conditions (Wainwright et al., 2008). In particular, small

quadrupedal mammals would be expected to match their high level of structural flexibility (flexed three-segmented limbs with low limb stiffness when running; Farley et al., 1993; Fischer et al., 2002) with high functional variation during locomotion. This inferred by the fact that quadrupeds have to coordinate their fore and hindlimbs, leading to higher control efforts than in bipeds. We therefore tested the prediction that even during *overall* steady locomotor speed, small mammals show frequent inter-step speed variations that follow a regular and stereotyped pattern.

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70 RESULTS

Despite a relatively constant overall locomotor speed in each trial, almost two-thirds of all observed step transitions (N=120) were subjected to an increase (N=46) or decrease (N=32) in locomotor speed associated with slight changes of ground reaction forces (GRF's; Fig. 1). Interestingly, kinematic parameters that discriminate for s<sub>0</sub> locomotor parameters were exclusively related to liftoff whereas those for s<sub>1</sub> emphasized touchdown (Figs. 2A & 3A-F, Table 1). The discriminant analysis of s<sub>0</sub> locomotor parameters showed that whole body braking forces at  $s_0$  tended to be higher when rats decelerated between  $s_0$  and  $s_1$  (DF2 in Fig. 2A; G1 vs. G3 & G2 vs. G4 in Fig. 3E-F). More noteworthy, however, is the finding that footfall order of a given step  $(s_1)$  is a consequence of characteristics of the preceding step  $(s_0)$ , and is thus highly predictable. Rats that displayed small whole body peak propulsive forces and a more extended hindlimb at s<sub>0</sub> liftoff touched down with the forelimb first in s<sub>1</sub>, regardless of acceleration or deceleration between so and s1 (DF1 in Fig. 2A; G1 vs. G2 and G3 vs. G4 in Fig. 3A-C; vice versa for hindlimb touchdown in s<sub>1</sub>). Hindlimb extension at s<sub>0</sub>, however, was greater with an increase in speed between s<sub>0</sub> and s<sub>1</sub> (DF2 in Fig. 2A; G1 vs. G2 and G3 vs. G4 in Fig. 3D; vice versa for decelerating steps). In summary, the hindlimb at s<sub>0</sub> liftoff tended to be relatively more extended if the rats accelerated between s<sub>0</sub> and s<sub>1</sub> and landed on the forelimb first at s<sub>1</sub> (G4 in Figs. 2A, 3A & 3D), in contrast to s<sub>0</sub> steps where rats decelerated between s<sub>0</sub> and s<sub>1</sub> and landed first on the hindlimb at  $s_1$  (G1 in Figs. 2A, 3A & 3D; t-test P=0.0015).

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The discriminant analysis of  $s_1$  locomotor parameters revealed that  $s_1$  has a higher whole body peak braking force and a less protracted hindlimb when the forelimb of a diagonal couplet touched down first, compared to a hindlimb-initiated trotting step (DF 1 in Fig. 2B; Fig. 3G-I; Table 1). Higher whole body peak braking forces when landing first on the forelimb are likely due to the location of the center of mass (COM), which lies behind the center of

pressure of the forelimb at touchdown (Fig. 4). This has a significant influence on inter-step speed adjustments: a rat that landed first on its forelimb was more likely to reduce locomotor speed between  $s_0$  and  $s_1$  (31% for the forelimb vs. 19% for the hindlimb). Furthermore, we found a trend towards greater forelimb protraction at  $s_1$  when the rats accelerated between  $s_0$  and  $s_1$  (DF2 in Fig. 2B; Fig. 3J). In order to maintain *overall* steady-speed locomotion, the rats switched frequently between footfall orders. For example, if  $s_1$  was net propulsive and had a forelimb-initiated diagonal couplet step, then the preceding step ( $s_0$ ) was likely to be initiated with a hindlimb touchdown regardless if  $s_0$  was net braking or net propulsive (Fig. 5).

**DISCUSSION** 

The use of frequent alterations in touchdown order between consecutive steps and the ability to adjust speed at each step shows that rats possess a remarkable level of structured variability in the coordination of their limbs during stable, terrestrial steady-speed locomotion. While such structured variability would clearly be advantageous for the flexibility needed during locomotion on rough terrain, its occurrence on a substrate lacking irregularities suggests that much of stable, terrestrial steady-speed locomotion in rats is mechanically controlled. Indeed, our statistical analyses revealed few parameters that discriminate between footfall orders. Those parameters include relative limb length as well as relative limb protraction and retraction – parameters that play a predominant role in self-stability during perturbed locomotion in bipeds (Geyer et al., 2005; Daley and Biewener, 2006; Seyfarth et al., 2008). We therefore suggest that these parameters play an overall important role during terrestrial locomotion.

Almost two-thirds of all observed net-propulsive steps  $(s_0)$  with the hindlimb touching the ground before the forelimb were followed by a net-braking step  $(s_1)$  with the forelimb touching the ground before the hindlimb (Fig. 5). This suggests that the frequent alterations in limb coordination and the frequent changes between net braking and net propulsive steps characterize the locomotion of small- to medium sized mammals. Despite moving at an *overall* constant steady-speed, however, landing first on the forelimb does not correlate *per se* with a net braking step and a net-braking step  $(s_0)$  *per se* is not followed by a net-propulsive step  $(s_1)$  and *vice versa*. Occasional deviations thus support the previous assumption that the sensory information transfer (e.g., limb posture and speed) occurs once every step to determine whether to adjust footfall order

and/or locomotor parameters (Daley, 2008). The neural control system thus seems to play an additional and significant role in locomotor stability, even on a substrate without irregularities.

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By pairing this functional variability with the structural flexibility of three-segmented limbs, small- to medium-sized quadrupedal mammals may have an advantage when navigating uneven substrates, which are frequent features of the landscape for mammals of this size. In addition, mechanical self-stabilizing mechanisms would clearly reduce the complexity of the (neural) control system. Further experiments are needed to investigate the interplay between limb coordination, locomotor stability and substrate characteristics. The high functional variability may also predispose these mammals to locomotor intermittency (relative short traveled distances between frequent periods of rest) rather than long-distance, steady-speed travel (Eilam, 2004). Hence, morphology and eco-relevant factors may best explain frequent speed adjustments in rats.

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# MATERIALS AND METHODS

# Animals and experimental setup

The Ohio University Institutional Animal Care and Use Committee approved animal care and experimental procedures. Data were obtained from five adult male Fischer 344 X Brown Norway rats (Rattus norvegicus, Berkenhout 1769; 421±29 g). Rats were separately caged with food and water ad libitum. Animals were filmed as they moved at their voluntary speed across a force-plate instrumented terrestrial trackway (length, 2200 mm; width: 150 mm) without irregularities. At least 20 trials per individual were recorded. From these trials we selected 5 trials that meet the following three criteria: (1) Each trial consists of at least 8 consecutive steps. The first and last two steps, respectively, are discarded to account for deceleration and acceleration steps during each trial. Trials for further data analysis consist, therefore, of at least 4 consecutive steps (mean N=5). (2) The gait used in each trial is a running trot (duty factor<50%; limb phase between 45-55%; see Gait Determination below). (3) Animals trot at a steady-speed (speed range was limited to  $\pm 10\%$  of mean velocity; see Spatio-temporal Gait Parameters below). In total, 150 steps were analyzed (speed range: 0.7-1.3 ms<sup>-1</sup>). The high variability in touchdown order and speed changes between these 150 steps were the basis of the following categorization. We focused on steps where both contralateral limbs touched the ground in series (this step was designated the reference step, s<sub>1</sub>). Steps with synchronous touchdown events were not considered to reduce the complexity of further analyses. The step preceding  $s_1$  is  $s_0$ . Finally,  $s_1$  steps were categorized into four groups (G) based on the nature of the speed change between  $s_0$  and  $s_1$  and which limb touched the ground first in  $s_1$ : (G1) speed reduction, hindlimb touchdown first; (G2) speed reduction, forelimb touchdown first; (G3) speed increase, hindlimb touchdown first; (G4) speed increase, forelimb touchdown first. Our analysis focused on two major events that are likely to be most important for speed adjustments between  $s_0$  and  $s_1$ ; namely,  $s_0$  lift off and  $s_1$  touchdown.

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## Analysis of spatio-temporal gait parameters

Metric and kinematic data were obtained with the Qualisys Motion Capture System (QTM, Gothenburg, Sweden). To film the rats across the length of the trackway, we placed two normal light high-speed cameras (Oqus 310 series, QTM) laterally and in series at a distance of 1.00 m to the direction of movement. Capture frequency was set to 125 Hz. Videos were calibrated and analyzed using the TRACKER software v.4.05 (www.opensourcephysics.org). For each trial, ipsilateral limbs facing the camera were analyzed at touchdown and liftoff. The distal tips of the third manual and pedal digits were digitized at touchdown and liftoff to obtain total stance duration (both contralateral limbs). The eye and the tail base were similarly digitized at touchdown and liftoff. Relative limb protraction (at touchdown) and retraction (at liftoff) were then calculated as the positions of the manual and pedal landmarks relative to the positions of the eye and the tail base, respectively (Nyakatura et al. 2008). Positive values in the forelimb indicate a more protracted limb whereas negative values in the hindlimb indicate a more retracted limb. The traveled distance of the eye (digitized at each second frame) was used to calculate mean locomotor speed for the complete trial as well as locomotor speed for each step. The latter was used to calculate changes in locomotor speed ( $\Delta v$ ) between  $s_0$  and  $s_1$ . Step transitions were subjected to an increase or decrease in locomotor speed if  $\Delta v \ge 0.02 \text{ms}^{-1}$ . Raw data were filtered using a 4<sup>th</sup> order low pass Butterworth filter with a cut off frequency of 25 Hz.

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# Analysis of kinetic locomotor parameters and whole body mechanics

Three-dimensional whole-body ground reaction forces (GRFs), comprising an anteroposterior, mediolateral and vertical component, were recorded at 1000 Hz using two Bertec force plates (part of a quad belt instrumented treadmill system); the 2mm gap between force plates did not influence locomotor behavior in the rats. Analog signals from the force plates were transferred directly to the Qualisys system *via* an analog digital board (Qualisys 64 channel A/D board, S/N

8124) and an amplifier (Bertec, AM-6800 signal converter). All data were exported into Excel and filtered using a 4<sup>th</sup> order low pass Butterworth filter with cut off frequencies between 20-50 Hz depending on the force component. Finally, the GRFs were analyzed and normalized to each animal's body weight. Kinetic data included whole body peak vertical, braking and propulsive force and associated impulses (mediolateral peak forces and impulses were not considered). To estimate the effect of vaulting and bouncing mechanics, we calculated fluctuations in the external mechanical energies and percentage energy recoveries over a step (Cavagna et al. 1977; see below).

## Analysis of kinetic locomotor parameters and whole body mechanics

GRFs were exported into a custom-made LabView program (National Instruments, Austin, TX, USA; Parchman et al., 2003). Accelerations of the center of mass (COM) in all three directions were calculated by dividing out body mass (body weight was first substracted from the vertical force). Velocities of the COM for each direction were then estimated by taking the first integration of acceleration (integration constant estimated as the mean value for each force record). These velocities were used to calculate kinetic energies ( $E_K = \frac{1}{2}mv^2$ , where m is body mass in kg and v is velocity in ms<sup>-1</sup>) in the vertical ( $E_{K-V}$ ), cranio-caudal ( $E_{K-CC}$ ), and medio-lateral ( $E_{K-ML}$ ) directions. Summing the three kinetic energies yields the total kinetic energy of the COM ( $E_{K-TOT}$ ). Changes in the vertical displacement of the center of mass (h) were determined by integrating vertical velocity (integration constant estimated as the mean vertical record) and were used to determine changes in gravitational potential energy during the step ( $E_P = mgh$ , where g is gravitational acceleration with 9.81 ms<sup>-2</sup>). The sum of  $E_{K-TOT}$  and  $E_P$  yields the total external mechanical energy ( $E_{M-TOT}$ ). Finally, we calculated percentage energy recoveries and phase shifts

#### Gait determination

of the fluctuations between  $E_K$  and  $E_P$  (Cavagna et al., 1977).

Duty factor (S) and limb phase (synonymous to diagonality; Cartmill et al. 1977) were used to identify running gaits used by the rats (Hildebrand, 1966). Duty factor for one limb refers to the percentage of stance duration of one complete stride cycle whereas limb phase refers to the time from the forelimb touchdown to the touchdown of the ipsilateral hindlimb (in percentage of the hindlimb stride cycle). Forelimb and hindlimb duty factors were used to calculate the duty factor index ( $S_{Index}$ =100  $S_{Hindlimb}$ / $S_{Forelimb}$ ; Cartmill et al. 1977).

Statistical Analyses	
SPSS (v16.0; IBM, Somers, NY, USA) was used for statistical analysis. We performed	two
separate discriminant function analysis on s <sub>0</sub> and s <sub>1</sub> locomotor parameters, including sta	ance
duration, duty factor index, relative limb protraction at touchdown, relative limb retraction	n at
liftoff, limb extension at touchdown and liftoff, phase shift, percentage energy recovery,	and
whole body peak vertical, braking and propulsive force and associated impulses, to identify	/ the
parameters that discriminate between all four groups (G1-G4). Variables that were consider	ered
significantly different displayed structure matrix coefficient loadings greater than 0.30.	The
significance level for all analyses was set at $P < 0.05$ .	
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AUTHOR CONTRIBUTION	
A.S. and A.R.B. conceived and designed the experiments and prepared the manuscript.	A.S.
performed the experiments and data analysis.	
COMPETING INTERESTS	
None.	
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Biknevicius, N.J. Stevens and S.M. Reilly).	•
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251	REFERENCES
252	Biewener, A. A. and Daley, M. (2007). Unsteady locomotion: integrating muscle function with
253	whole body dynamics and neuromuscular control. J. Exp. Biol. 210, 2949-2960.
254	Blickhan, A., Seyfarth, A., Geyer, H., Grimmer, S., Wagner, H. and Günther, M. (2010).
255	Intelligence by mechanics. Phil. Trans. R. Soc. A 365, 199-220.
256	Cartmill, M., Lemelin, P. and Schmitt, D. (1977). Support polygons and symmetrical gaits in
257	mammals. Zool. J. Linn. Soc. 136, 401-420.
258	Cavagna, G. A., Heglund, N. C. and Taylor, R. C. (1977). Mechanical work in terrestrial
259	locomotion: two basic mechanisms for minimizing energy expenditure. Am. J. Physiol.
260	<b>233</b> , 243-261.
261	Daley, M. and Biewener, A. A. (2006). Running over rough terrain reveals limb control for
262	intrinsic stability. PNAS, <b>103</b> , 15681-15686.
263	Daley, M. (2008). Biomechanics: Running over uneven terrain is a no-brainer. Current
264	Biology 18, R1064-R1066.
265	Eilam, D. (2004). Locomotor activity in common spiny mice (Acomys cahirinuse): The effect of
266	light and environmental complexity. BMC Ecology 4, 16-26.
267	Farley, C. T., Glasheen, J. and McMahon, T. A. (1993). Running springs: speed and animal
268	size. J. Exp. Biol. 185, 71-86.
269	Fischer, M. S., Schilling, N., Schmidt, M., Haarhaus, D. and Witte, H. (2002). Basic limb
270	kinematics of small therian mammals. J. Exp. Biol. 205, 1315-1338.
271	Full, R. J. and Koditschek, D. E. (1999). Templates and anchors: neuromechanical hypotheses
272	of legged locomotion on land. J. Exp. Biol. 202, 3325-3332.
273	Full, R. J., Kubow, T., Schmitt, J., Holmes, P. and Koditschek, D. (2002). Quantifying
274	dynamic stability and maneuverability in legged locomotion. Integ. Comp. Biol. 42, 149-
275	157.
276	Geyer, H., Seyfarth, A. and Blickhan, R. (2005). Spring-mass running: simple approximate
277	solution and application to gait stability. J. Theor. Biol. 232, 315-328.
278	Grimmer, S., Michael, E., Günther, M., and Blickhan, R. (2008). Running on uneven ground:
279	leg adjustment to vertical steps and self-stability. J. Exp. Biol. 211, 2989-3000.
280	Hiebert, G. W. and Pearson, K. G. (1999). Contribution of sensory feedback to the generation
281	of extensor activity during walking in the decerebrate cat. J. Neurophysiol. 81, 758-770.

283	<b>Hildebrand, M.</b> (1966). Analysis of the symmetrical gaits of tetrapods. <i>Folia Biotheoretica</i> <b>6</b> ,
284	9–22.
285	Hooper, S. (2012). Body size and the neural control of movement. Current Biology 22, 318-322
286	Nyakatura, J. A., Fischer, M. S. and Schmidt, M. (2008). Gait parameter adjustments of
287	cotton-top tamarins (Saguinus oedipus, Callitrichidae) to locomotion on inclined arboreal
288	substrates. Am. J. Phys. Anthropol. 135, 13-26.
289	Parchman, A. J., Reilly, S. M. & Biknevicius, A. R. (2003). Whole-body mechanics and
290	gaits in the gray short-tailed opossum Monodelphis domestica: integrating patterns of
291	locomotion in a semi-erect mammal. J. Exp. Biol. 206, 1379-1388.
292	Seyfahrt, A., Geyer, H., Günther, M. and Blickhan, R. (2008). A movement criterion for
293	running. J. Biomech. 35, 649-655.
294	Wainwright, P. C., Metha, R. S. and Higham, T. E. (2008). Stereotype, flexibility and
295	coordination: key concepts in behavioral functional morphology. J. Exp. Biol. 211; 3523-
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299	FIGURE LEGENDS
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Figure 1 Representative ground reaction force profiles of five consecutive steps of a trotting rat at steady-speed (1.30±0.02 ms<sup>-1</sup>) across a terrestrial substrate. Note slight fluctuations in force profile magnitude and shape.

**Figure 2** Results of discriminant function analyses on locomotor parameters of  $s_0$  (left) and  $s_1$  (right). Groups (1-4) used in each analysis are based on touchdown order and inter-step speed adjustments (see Materials and methods). For each function (DF), the best discriminating variables with structure matrix loadings >0.3 are listed in parentheses.  $s_0$ -preceding step;  $s_1$ -reference step; FL-forelimb; HL-hindlimb; PROTR-protraction; RETR-retraction; EXT-extension; TD-touchdown; LO-lift off; BRIMP-braking impulse; PBF-peak braking force; PPF-peak propulsive impulse.

**Figure 3** Results of statistical analyses (*t-test*) performed on locomotor parameters with discriminant function analyses structure matrix loadings higher than 0.3 (see Figure 2; Table 1). Asterisks indicate significant differences between groups G1-G4 (e.g., G1 vs. G2; DF1 of  $s_0$ ; P<0.05). (A-C) G1 vs. G2; G3 vs. G4; DF2 of  $s_0$ ; (D-F) G1 vs. G3; G2 vs. G4; DF1 of  $s_0$ ; (G-I) G1 vs. G2; G3 vs. G4; DF1 of  $s_1$ ; (J) G1 vs. G3; G2 vs. G4; DF2 of  $s_1$ . Labeled as in Figure 2 and Table 1.

**Figure 4** Drawings of a trotting rat from still images at touchdown with the forelimb (A) and the hindlimb first (B), respectively. Note that the center of mass (COM; gray dot) is located behind and in front of the limb that touches the ground first, respectively (position of the COM; A.S. personal observation).

**Figure 5** Proposed model of the relationship between touchdown order, inter-step speed adjustments and net anteroposterior impulses (synchronous touchdowns are not included). For example, if  $s_1$  was net propulsive and had a forelimb touchdown that occurred before the hindlimb touchdown (FL first) then the preceding step  $s_0$  would have been a hindlimb touchdown first (HL first) regardless if  $s_0$  was net braking (29%) or net propulsive (71%).

**Table 1** Discriminant analysis structure matrices, eigenvalues, and percentages of variances explained by each function of  $s_0$  and  $s_1$ .

		$s_0$	-1-		$s_1$	
	DF1	DF2	DF3	DF1	DF2	DF3
Eigenvalues	2.666	0.865	0.230	6.483	0.846	0.617
% of Variance	70.9	23.0	6.1	81.6	10.6	7.8
Cumulative %		93.9	100.0		92.2	100.0
<b>Canonical Correlation</b>	0.853	0.681	0.433	0.931	0.677	0.618
P	0.010	0.588	0.953	< 0.0001	0.175	0.309
$HL_{PROTR}$	0.019	0.222	0.071	0.326	0.259	0.285
$HL_{EXT-TD}$	0.039	-0.135	0.378	-0.110	0.021	0.110
$HL_{RETR}$	0.092	-0.114	0.173	-0.152	-0.092	0.083
HL <sub>EXT-LO</sub>	-0.447	0.365	0.253	0.185	0.047	0.029
$FL_{PROTR}$	0.065	0.098	0.220	-0.108	0.414	-0.164
$FL_{EXT-TD}$	-0.201	-0.096	-0.048	0.134	0.239	-0.048
$FL_{RETR}$	0.309	-0.151	0.146	-0.148	-0.090	0.184
$FL_{EXT-LO}$	0.069	-0.173	0.282	-0.174	0.227	0.122
BRIMP	0.022	0.409	0.001	0.326	-0.269	0.363
PBF	-0.029	0.541	-0.050	0.408	-0.271	0.411
PRIMP	0.066	0.162	-0.433	-0.030	-0.229	0.190
PPF	0.347	0.219	-0.441	-0.097	-0.185	0.254
VIMP	-0.112	0.055	-0.046	-0.035	0.211	0.046
PVF	0.084	-0.187	-0.008	-0.125	-0.207	0.083
%Recovery	-0.256	0.167	-0.122	0.285	-0.173	-0.297
PS	-0.015	0.210	-0.263	0.198	-0.152	-0.234
SD	-0.037	-0.055	0.008	-0.034	0.267	0.048
DFI	-0.127	-0.203	0.096	0.088	0.150	-0.196

s<sub>0</sub>-preceding step; s<sub>1</sub>-reference step; FL-forelimb; HL-hindlimb; PROTR-protraction; RETR-retraction; EXT-extension; TD-touch down; LO-lift off; BRIMP-braking impulse; PBF-peak braking force; PRIMP-propulsive impulse; PPF-peak propulsive impulse; VIMP-vertical impulse; PVF-peak vertical force; PS-phase shift; SD-stance duration; DFI-duty factor index.









