

## RESEARCH ARTICLE

# Minor contributions of the maxillary sinus to the air-conditioning performance in macaque monkeys

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## ABSTRACT

The nasal passages mainly adjust the temperature and humidity of inhaled air to reach the alveolar condition required in the lungs. By contrast to most other non-human primates, macaque monkeys are distributed widely among tropical, temperate and subarctic regions, and thus some species need to condition the inhaled air in cool and dry ambient atmospheric areas. The internal nasal anatomy is believed to have undergone adaptive modifications to improve the air-conditioning performance. Furthermore, the maxillary sinus (MS), an accessory hollow communicating with the nasal cavity, is found in macaques, whereas it is absent in most other extant Old World monkeys, including savanna monkeys. In this study, we used computational fluid dynamics simulations to simulate the airflow and heat and water exchange over the mucosal surface in the nasal passage. Using the topology models of the nasal cavity with and without the MS, we demonstrated that the MS makes little contribution to the airflow pattern and the air-conditioning performance within the nasal cavity in macaques. Instead, the inhaled air is conditioned well in the anterior portion of the nasal cavity before reaching the MS in both macaques and savanna monkeys. These findings suggest that the evolutionary modifications and coetaneous variations in the nasal anatomy are rather independent of transitions and variations in the climate and atmospheric environment found in the habitats of macaques.

**KEY WORDS:** Computational fluid dynamics, Humidity, Nasal airflow, Nasal cavity, Primates, Temperature

## INTRODUCTION

Macaque monkeys, genus *Macaca*, are a group of Old World monkeys in the family Cercopithecidae (Fooden, 1980; Fleagle, 2013). At present, macaques are distributed widely in western to eastern Asia and in a restricted region of North Africa (Fooden, 1980; Smith et al., 2005). They show the second-largest geographic distribution after humans among primates. This group probably arose in northern Africa in the Late Miocene, before expanding their distribution into Eurasia during the Late Miocene and then dispersing to East Asia by the Late Pliocene (Delson, 1980; Alba

et al., 2014). Their adaptive radiation resulted in their successful colonization of more varied climates and ecological environments compared with other Old World monkeys (Fleagle, 2013). In particular, the Japanese macaque, *Macaca fuscata*, expanded its distribution throughout the Japanese Archipelago from subtropical into subarctic zones, which are the highest latitudes inhabited by non-human primates (Fooden, 1980). These ecogeographical features are reflected partly by the broad morphological variations in terms of body size and the shapes of surface features within this genus (Fooden and Albrecht, 1993; Pan and Oxnard, 2000; Ito et al., 2014, 2015).

The nasal cavity allows the inhaled air to flow from the external nostril into the pharyngeal region (Cole, 1982; Elad et al., 2008). The nasal cavity conditions the respiratory air, as well as performing other functions such as olfactory sensing, dust filtering and voice resonance (Cole, 1982; Elad et al., 2008). The nasal cavity behind the nasal vestibule is divided into three thin channels, which are referred to as the inferior, middle and superior meatuses with the olfactory cleft. The three meatuses are separated by two major thin bony plates that are covered by respiratory mucosa, which are referred to as the conchae or turbinates (Cave, 1973; Cole, 1982; Harkema et al., 1987; Elad et al., 2008). The inhaled air flows over the mucosal surface, exchanges heat and water with the mucosal tissues and is adjusted to the alveolar condition, i.e. fully saturated at body temperature, before it reaches the lung. This means that increasing the surface area of the respiratory mucosa improves the air-conditioning performance. Indeed, the bony nasal cavity is widened and enlarged in the population of Japanese macaques that inhabit the northern (colder and drier) region compared with those in the southern (warmer and wetter) regions (Rae et al., 2003). Inadequate air conditioning damages the mucosal tissues of the respiratory system and also impairs the respiratory performance, thereby endangering the health and affecting the survival of animals. The nasal cavity anatomy is often regarded as being evolutionarily sensitive to the ambient atmospheric conditions of the habitat in macaques (Rae et al., 2003; Márquez and Laitman, 2008). Thus, the current ecogeographical range of macaques may depend partly on evolutionary modifications in their nasal anatomy to improve the air-conditioning performance.

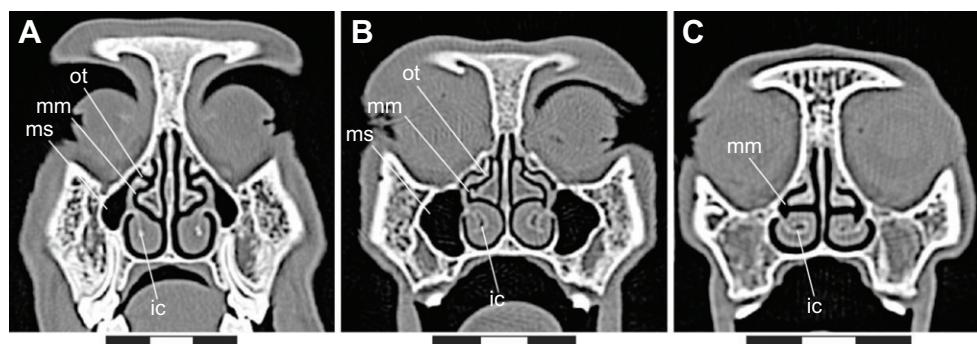
The maxillary sinus (MS) is one of the paranasal sinuses, which communicates with the middle meatus of the nasal cavity via a narrow opening called the ostium and pneumatizes the maxilla (Rae and Koppe, 2004; Rossie, 2008). This bony sinus is lined with a respiratory mucosa that extends from the nasal cavity through the ostium (Rae and Koppe, 2004; Rossie, 2008). MS pneumatization is always found in macaques and sometimes in baboons and gelada (*Papio* and *Theropithecus*), whereas it is absent in other extant Old World monkeys (Koppe and Ohkawa, 1999; Nishimura et al., 2014). This feature is believed to have arisen independently in these lineages as the paranasal sinuses, including the MS, were lost once

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**Fig. 1.** Frontal computed tomography (CT) scans. (A) Japanese macaque, *Macaca fuscata* (Mff765; CT scan id, PRICT-369); (B) rhesus macaque, *Macaca mulatta* (Mm1701; PRICT-394); and (C) savanna monkey, *Chlorocebus aethiops* (Ca14; PIRECT-27).

Abbreviations: ic, inferior concha; mm, middle meatus; ms, maxillary sinus; ot, ostium. The scale is in centimeters.

in a common ancestor of extant Old World monkeys (Rae et al., 2002). The performance of the air conditioning depends mainly on how the air flows through the nasal cavity (Lindemann et al., 2004; Naftali et al., 2005; Kumahata et al., 2010; Hanida et al., 2013). The structures in the nasal cavity, especially in its anterior region, have major effects on the air-conditioning performance in humans (Lindemann et al., 2004; Naftali et al., 2005; Kumahata et al., 2010; Hanida et al., 2013). Nevertheless, in macaques, the MS topological differences suggests it has a functional role in air conditioning (Márquez and Laitman, 2008), and the airflow in and out of the MS could affect the airflow within the nasal cavity, which has some topological differences from that in humans.

In this study, we evaluated air-conditioning performance using computational fluid dynamics (CFD) simulations based on a three-dimensional (3D) topological model of the nasal cavity and MS derived from the computed tomography (CT) scans of six macaques (including four *M. fuscata* Blyth 1875 and two *M. mulatta* Zimmermann 1780) and a savanna monkey (*Chlorocebus aethiops* Linnaeus 1758) (Fig. 1; supplementary material Table S1). To evaluate the potential contribution of the MS to nasal passage airflow in macaques, we also generated nasal topology models where the MS was virtually removed for each macaque subject, i.e. no-MS model. We hypothesized that

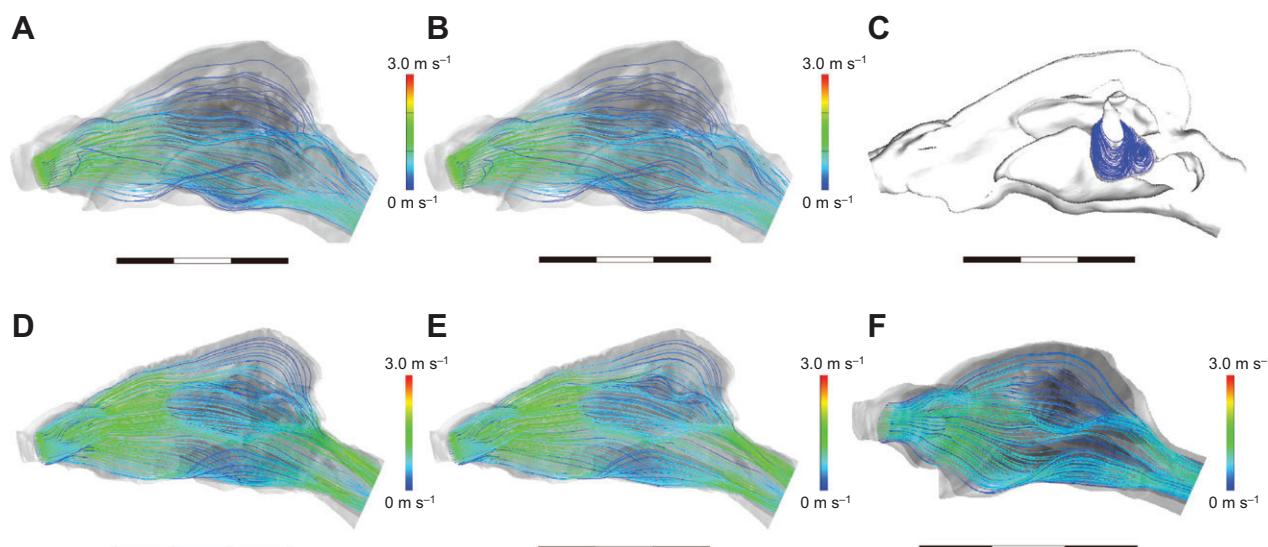
possible improvements in the air-conditioning performance and the contribution of the reacquired MS in macaques may have facilitated their successful adaptive radiation into various habitats.

## RESULTS

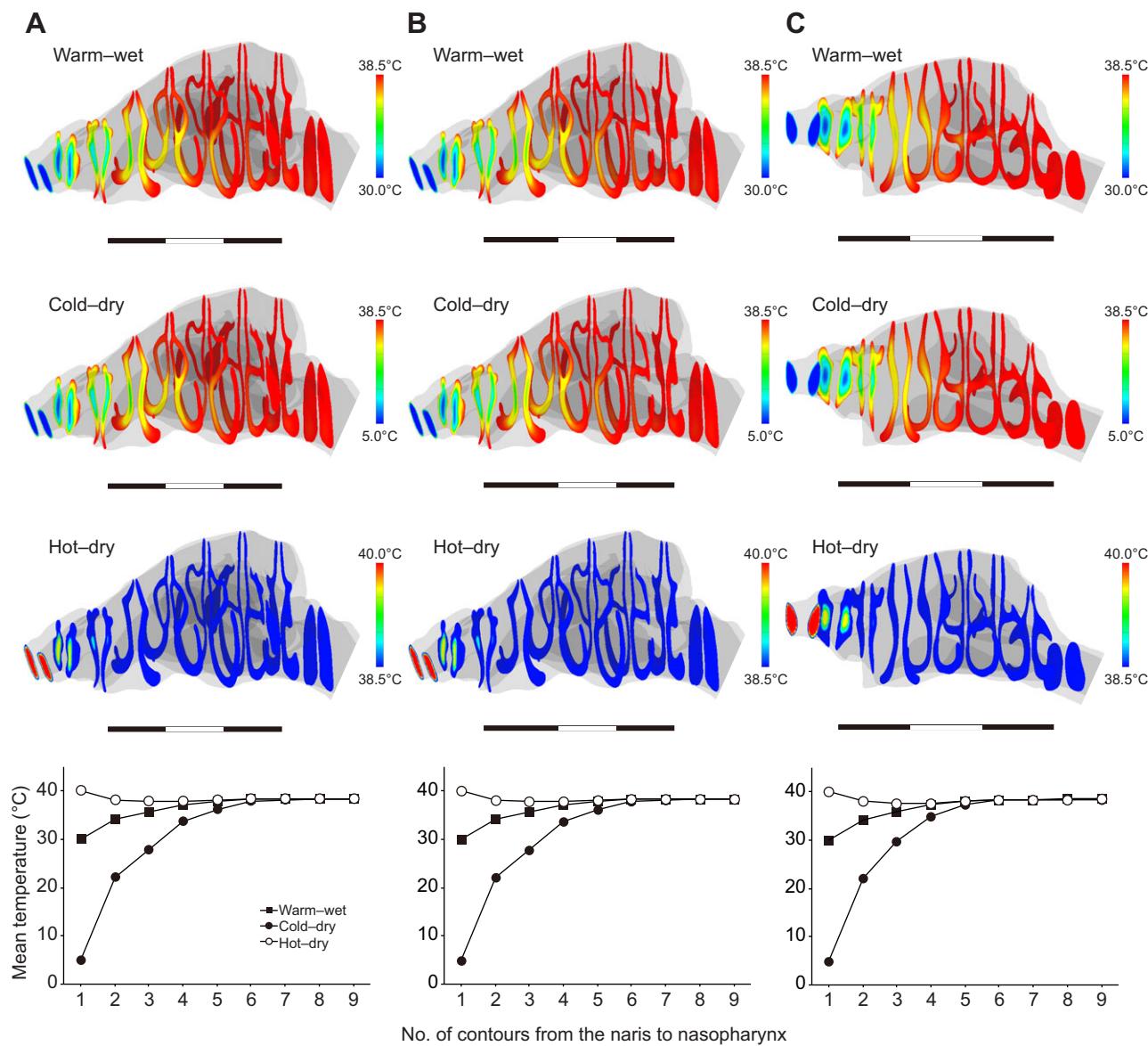
Visualizations in airflow and distributions of temperature and humidity are for one representative subject of the macaques studied (Figs 2–4), because all subjects here showed comparable airflow pattern and air-conditioning performance. The illustrations in the other subjects are provided in the supplementary material (supplementary material Figs S1–S3).

The inhaled air flowed almost horizontally and straight from the external nostril through the pharyngeal region, and the flow usually had a greater velocity through the middle regions compared with the peripheral regions of the nasal meatuses in macaques (Fig. 2A,D; supplementary material Fig. S1). The CFD simulations using the no-MS model demonstrated that the airflow was almost the same as that in the normal model for each macaque (Fig. 2B,E; supplementary material Fig. S1). Furthermore, similar airflow patterns were also found in a savanna monkey, which lacks the MS (Fig. 2F), and there were no noticeable distinctions between the two genera.

The size of the MS was restricted in Japanese macaques (average of 346 mm<sup>3</sup>) compared with rhesus macaques (average of 1254 mm<sup>3</sup>;



**Fig. 2.** Airflow and flow velocity in the nasal cavity and within the maxillary sinus. (A–C) The airflow in the nasal cavity simulated with the normal model (A) and the no-maxillary sinus (MS) model (B), and simulated within the maxillary sinus (C) for a Japanese macaque, *M. fuscata* (Mff765; PIRECT-369). (D,E) The airflow in the nasal cavity simulated with the normal model (D) and the no-MS model (E) for a rhesus macaque, *M. mulatta* (Mm1715m; PIRECT-395). (F) The airflow for a savanna monkey, *C. aethiops* (Ca14; PIRECT-27). The streamline indicates the airflow direction and velocity distributions throughout the nasal passage. The streamline number reflects the airflow volume. The scale is in centimeters.



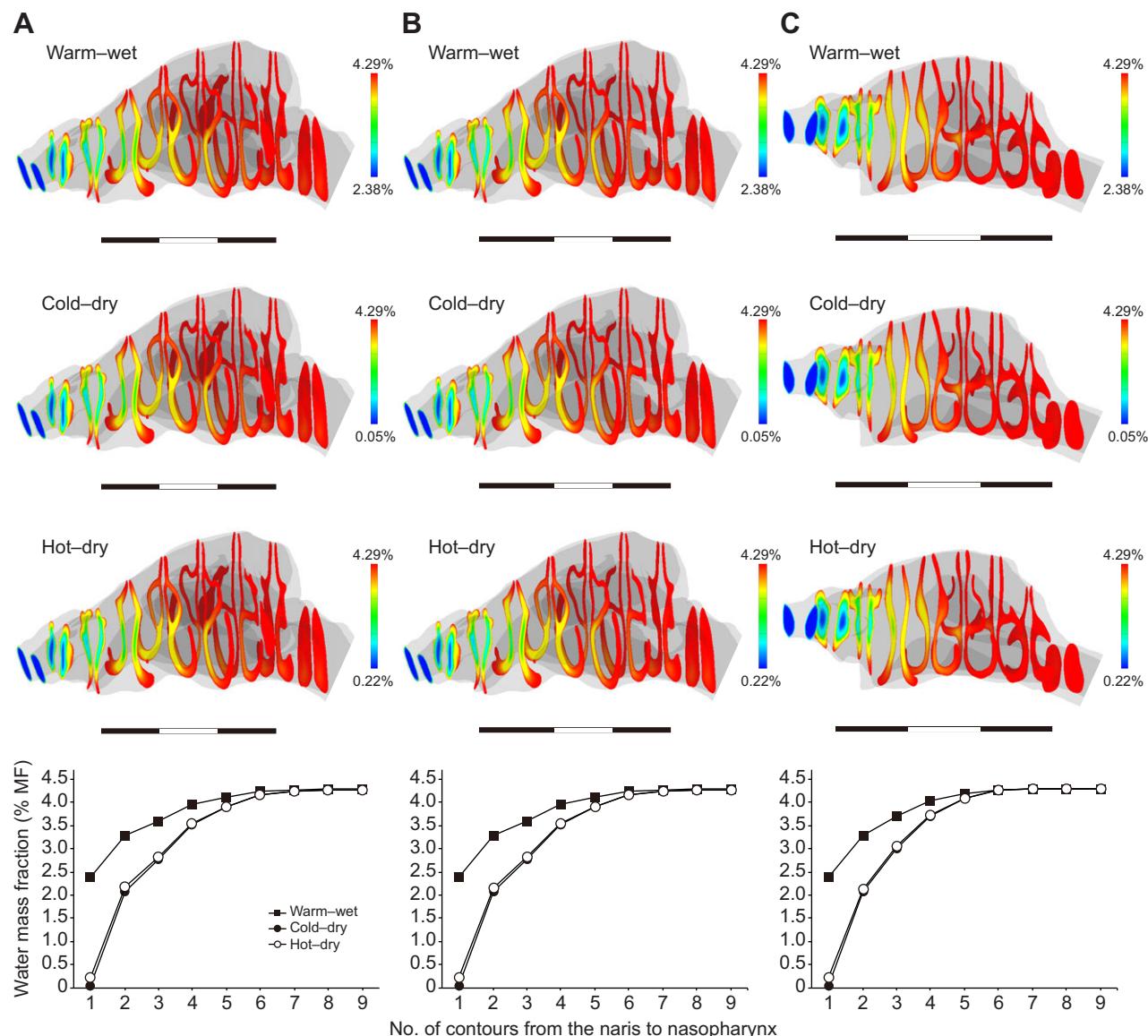
**Fig. 3. Temperature distribution in the nasal passage.** (Top) The contours represent the temperature distribution at each level from the nares to the nasopharynx, which were simulated with the normal model (A) and the no-MS model (B) for Japanese macaques, *M. fuscata* (Mff765; PRICT-369), and for a savanna monkey, *C. aethiops* (Ca14; PRICT-27) (C). The mean temperature values for each contour from the nostril to nasopharynx (bottom) indicate the performance when adjusting the temperature to 38.5°C. The scale is in centimeters.

Fig. 1). There was one ostium for each MS in all the subjects used here, and this varied in shape from almost circular to a horizontally long ellipse. Regardless of this difference in MS anatomy, the inhaled air usually entered the MS from the posterior side of the ostium, which produces slow vortices within the MS, and it then exited the MS via the anterior side (Fig. 2C; supplementary material Fig. S1). The flow within the MS reached up to  $0.0005 \text{ m s}^{-1}$ , which was far slower ( $>2000$  times) than that in the nasal cavity at the level of the ostium (average of  $1.02 \text{ m s}^{-1}$ ) in both species of macaque.

In the macaques and a savanna monkey, the temperature of the inhaled air was adjusted almost fully to 38.5°C, which is the temperature of the nasal organ set here, in the nasopharyngeal region with all three ambient atmospheric conditions (Table 1, Fig. 3A,C; supplementary material Fig. S2). We found that the air was conditioned rapidly in the anterior region of the nasal cavity in these species (Fig. 3A,C; supplementary material Fig. S2). The air

was adjusted almost fully to 38.5°C at the level of the ostium of the MS in both species of macaque, and the adjusted air then entered the MS (Fig. 3A; supplementary material Fig. S2). This adjustment in temperature was also obtained in the no-MS models of macaques (Table 1, Fig. 3B; supplementary material Fig. S2), and there were few differences in the temperature distributions of the normal and no-MS models, i.e. only up to 0.5°C in the mean value for the same frontal contour (Table 1, Fig. 3A,B; supplementary material Fig. S2).

The mass fraction of water (MF) was also adjusted rapidly toward saturation at a given temperature, and it was fully saturated at 4.29% MF when the temperature was adjusted to 38.5°C (i.e. at 100% relative humidity, RH) in the anterior portion of the nasal cavity, which was the case in all atmospheric conditions for macaques and savanna monkeys (Table 1, Fig. 4A,C; supplementary material Fig. S3). Thus, fully saturated air reached the ostium of the MS in



**Fig. 4. Water mass distributions in the nasal passage.** (Top) The contours represent the distribution of the water mass fraction (MF) at each level from the nares to the nasopharynx, which were simulated with the normal model (A) and the no-MS model (B) for Japanese macaques, *M. fuscata* (Mff765; PRICT-369), and for a savanna monkey, *C. aethiops* (Ca14; PRICT-27) (C). The mean water mass values for each contour from the nostril to nasopharynx (bottom) indicate the performance of water vapor transport in the inhaled air to 4.29% MF. The scale is in centimeters.

macaques (Fig. 4A; supplementary material Fig. S3). The same saturation performance was also obtained in the no-MS models of macaques (Table 1, Fig. 4B; supplementary material Fig. S3), and there were few differences between the normal and no-MS models, i.e. up to 0.08% MF in the mean value for the same frontal contour (Table 1, Fig. 4A,B; supplementary material Fig. S3).

## DISCUSSION

Our CFD simulations demonstrated that the MS has few positive or negative effects on airflow for air conditioning within the nasal cavity of macaques. These minor contributions are probably attributable to the small ostium and the thin and long channel between the nasal cavity and the hollow of the MS (Fig. 1), and not to the volume of the MS. The airflow from the MS is too highly restricted and slow to modify the airflow within the nasal cavity in macaques, as seen in humans (Xiong et al., 2008; Na et al., 2012;

Zhu et al., 2012). Thus, our bioengineered approach suggests that the reacquisition of the MS and its later anatomical modifications are functionally unrelated to the performance of air conditioning and the dispersal of macaques into cooler and drier environments.

Many hypotheses have been proposed based on comparative morphology approaches to explain the physiological or mechanical functions related to the paranasal sinuses including the MS, e.g. cooling and regulation of the brain or orbital temperature, reactive reduction of the masticatory load on the cranium, acoustic modifications of nasalized voices, and air conditioning (Shea, 1977; Rae et al., 2003; Rae and Koppe, 2008; Curtis and Van Valkenburgh, 2014; Van Valkenburgh et al., 2014). The paranasal sinuses are often thought to reduce the weight of the cranium and save bony materials by eliminating unnecessary bony resources (Rae and Koppe, 2004; Smith et al., 2005; Zollikofer and Weissmann, 2008). Although its biological advantages are still argued, the paranasal

**Table 1.** Mean values of temperature and water mass fraction at the nasopharyngeal level

Subjects	Warm-wet		Cold-dry		Hot-dry	
	Temperature (°C)	MF (%)	Temperature (°C)	MF (%)	Temperature (°C)	MF (%)
<i>Japanese macaques, Macaca fuscata</i>						
Mff765						
MS	38.5	4.28	38.4	4.27	38.5	4.27
No-MS	38.5	4.28	38.4	4.27	38.5	4.27
Mff963						
MS	38.4	4.27	38.3	4.25	38.4	4.25
No-MS	38.4	4.27	38.3	4.25	38.4	4.25
Mff1859						
MS	38.5	4.29	38.5	4.29	38.5	4.29
No-MS	38.5	4.30	38.5	4.30	38.5	4.30
Mff2115						
MS	38.7	4.30	38.5	4.30	38.5	4.30
No-MS	38.5	4.30	38.5	4.29	38.5	4.29
<i>Rhesus macaques, Macaca mulatta</i>						
Mm1701						
MS	38.5	4.30	38.5	4.30	38.5	4.30
No-MS	38.5	4.30	38.5	4.30	38.5	4.30
Mm1715						
MS	38.5	4.30	38.5	4.30	38.5	4.30
No-MS	38.5	4.29	38.5	4.29	38.5	4.29
<i>Savanna monkey, Chlorocebus aethiops</i>						
Ca14	38.5	4.29	38.5	4.29	38.5	4.29

MF, water mass fraction; MS, maxillary sinus.

sinus is believed to develop opportunistically from the nasal meatus if there are few structural disturbances, in that the pneumatization begins and progresses (Zollikofer and Weissmann, 2008; Smith et al., 2010). The paranasal sinus might develop and form as a spandrel, i.e. a feature passively formed by functional surrounding structures, but its evolutionary retention and inheritance in a given lineage should confer some evolutionary advantages that conquer some known disadvantages this feature has, e.g. risk of sinus inflammation, polyps, and aplasia and hypoplasia, which produce malformation in the cheek surface and orbital floor (Dumonceaux et al., 1997; Koppe et al., 2006; Zimmermann et al., 2011; Nishimura and Ito, 2014). The advantages of such a spandrel-like feature are probably varied for different clades. The paranasal sinus is absent from most clades of the Old World monkeys, but the MS re-emerged in the crown lineage of macaques since its ancestral loss from Old World monkeys (Koppe and Ohkawa, 1999; Rae et al., 2002; Nishimura et al., 2014). Thus, the MS might confer specific functional advantages in macaques. Future analyses of function, like the present approach, are expected to explain any adaptive significance of this feature for the crown group of macaques.

Furthermore, our study supports a scenario where macaques probably inherited a primitive faculty with excellent air conditioning, which facilitated their successful radiation into the temperate zone. The nasal cavity anatomy is often regarded as being evolutionarily sensitive to the ambient atmospheric conditions of a habitat in a given clade (Franciscus and Long, 1991; Rae et al., 2003; Márquez and Laitman, 2008), and thus the nasal region is often regarded as an independent functional module of the skull bony morphology, i.e. this region can be modified independently of the surrounding bony regions while maintaining appropriate physiological functions (Anton, 1989). Nevertheless, the inhaled air is fully conditioned in the anterior portion of the nasal cavity in both macaques and savanna monkeys. These findings suggest that evolutionary modifications in the nasal anatomy, even in the anterior portion, can also be explained in terms of physiological or structural functions, as well as of air

conditioning, at least in Old World monkeys. This view is also supported by recent morphological findings, which show that modifications of the nasal cavity are integrated with those in the neighboring cranial functional modules in humans and macaques, including the dentition, orbits and facial surfaces (Bastir and Rosas, 2013; Ito et al., 2015). Thus, the morphological variation in the nasal region might be only a weak response to the air-conditioning function in Old World monkeys including macaques.

## MATERIALS AND METHODS

### Subjects and CT scanning

Six macaques (four female Japanese macaques, *M. fuscata*, and one male and one female rhesus macaque, *M. mulatta*) and one savanna monkey (*C. aethiops*, male), which were reared at the Primate Research Institute, Kyoto University (KUPRI), Inuyama, Japan, were scanned using a CT scanner (Asteion Premium 4, Toshiba Medical Systems Co.) at the same institute (Fig. 1; supplementary material Table S1). Rhesus macaques are distributed in tropical and subtropical areas from western to eastern Asia. The savanna monkey is an Old World monkey that lacks a MS, and it is distributed in tropical Africa. All of the subjects were anesthetized intramuscularly with 2.5 mg ketamine hydrochloride (Ketalar®, Daiichi Sankyo Propharma, Tokyo, Japan) and 0.1 mg medetomidine hydrochloride (Domitor®, Nippon Zenyaku Kogyo Co. Ltd, Fukushima, Japan) per kilogram body weight before CT scanning. All of the experiments were performed in accordance with the third edition of the Guidelines for the Care and Use of Laboratory Primates at KUPRI, and the experimental protocol was approved by the Animal Welfare and Care Committee of the same institute.

All of the CT scans obtained in this study came from subjects without any history of surgery and that had few abnormal traits in their heads, and few artifacts distorted the images of the nasal region. The scans were registered under PRCT number (see supplementary material Table S1) and are available via the website of the Digital Morphology Museum of KUPRI (dmm.pri.kyoto-u.ac.jp/archive/).

### Reconstruction of nasal topology models

Voxel data for the nasal cavity and MS anatomy were reconstructed from the CT scans (Kumahata et al., 2010; Hanida et al., 2013). The black areas represent air filling the nasal cavity, and the MS was extracted first using Avizo

7 (FEI Visualization Sciences Group, Hillsboro, OH, USA) based on a threshold of brightness, and the voxel data were reconstructed. After converting the voxel data into STereoLithography (STL) data, they were modified into data that represented a smooth surface using Magics 9.5 (Materialize Inc., Leuven, Belgium). Finally, a tetrahedron mesh with a mesh size of  $\Delta x = 3.0 \times 10^{-3}$  mm was generated from the modified STL data using Gambit 2.4 (ANSYS Inc., Canonsburg, PA, USA). The computational meshes had 1–3 million tetrahedral cells. The present solutions were evaluated independently from the mesh size: there were few differences between the solutions with a mesh size of  $\Delta x = 0.18$  to  $0.40 \times 10^{-3}$  mm (the minimum size depends on the STL data size in each subject), i.e. up to 0.10% MF and  $1.0^\circ\text{C}$  in the mean value for the same frontal contour at the anterior nasal region, and up to 0.01% MF and  $0.0^\circ\text{C}$  at the posterior nasal and nasopharyngeal regions.

To evaluate the potential contributions of the MS to nasal passage airflow in macaques, we also generated a no-MS model from the original tetrahedron mesh data for each subject.

### Calculation methods

We performed steady-state analyses to examine the airflow, where the turbulence model was not employed. A steady simulation is reasonable under a normal breathing frequency and flow rate in the resting stage in humans (Swift and Proctor, 1977; Hornung et al., 1987; Hahn et al., 1993; Schreck et al., 1993; Keyhani et al., 1995; Dooryl et al., 2008; Kumahata et al., 2010; Hanida et al., 2013). The maximum Reynolds numbers ranged from 85 to 555 at the external nostrils in the subjects used here, calculated with estimates of the inhaled air velocity in the resting stage. They are lower than the critical Reynolds number (Swift and Proctor, 1977; Delson, 1980; Elad et al., 2008). The nasal flow was regarded as being mostly laminar in the resting stage of the subject used here. The Strouhal number value for the system was less than 0.25 (Dooryl et al., 2008). Moreover, the Womersley number for human breathing is small, thereby indicating that any inertial effects on the flow pattern may be regarded as negligible (Dooryl et al., 2008; Spence et al., 2012). We used the CFD simulation model developed by Hanida et al. (2013) to model an incompressible, viscous, laminar airflow in the nasal cavity with heat and water transport. The equations were solved using the fluid simulation software FLUENT 6.3 (ANSYS, Inc.).

The simulations were governed by the Navier–Stokes equation, i.e. the conservation of momentum equation (Eqn 1), by the conservation of mass equation (Eqn 2), by the transport of energy equation (Eqn 3) and by the transport of the mass fraction of water equation (Eqn 4):

$$\rho \left\{ \frac{\partial \mathbf{u}}{\partial t} + (\mathbf{u} \cdot \nabla) \mathbf{u} \right\} = -\nabla p + \mu \nabla^2 \mathbf{u}, \quad (1)$$

$$\nabla \cdot \mathbf{u} = 0, \quad (2)$$

$$pC_p \left\{ \frac{\partial T}{\partial t} + (\mathbf{u} \cdot \nabla) T \right\} = K \nabla^2 T, \quad (3)$$

$$\frac{\partial F}{\partial t} + (\mathbf{u} \cdot \nabla) F = D \nabla^2 F, \quad (4)$$

where  $t$ ,  $\mathbf{u}$ ,  $p$ ,  $\rho$ ,  $\mu$ ,  $K$ ,  $T$ ,  $C_p$ ,  $F$  and  $D$  denote time, velocity, pressure, density, kinematic viscosity, thermal conductivity, temperature, specific heat, the mass fraction of water and the mass diffusion coefficient, respectively. We regarded a solution as being of steady state, after  $T$  advanced, i.e. we repeated the steps of calculation sufficiently.

### Wall model for heat and water exchange

Heat and water are exchanged via the wall of the nasal cavity and the MS (if present). The wall comprises a vascular layer and mucous membrane. The wall was modeled as the organ and membrane layers (supplementary material Fig. S4) to simulate the exchange of heat and water from the vascular layer to the air via the mucous membrane (Hanida et al., 2013). The mucous membrane includes membrane epithelia, nasal glands, blood vessels and capillary blood vessels (Lang, 1989), and thus it varies in thickness between 0.3 and 5 mm, according to its location. The model comprised a smooth surface with a constant thickness of 0.5 mm, which was specified to simulate the actual performance in humans, after Hanida et al. (2013). Thus, the predicted air-conditioning performance may be slightly

worse than that actually found in small-bodied monkeys, which have a thinner mucous membrane, making the heat and water exchange efficient compared with that for the thick mucous membrane in humans. The optimum solution values for the temperature and humidity of the air were calculated by setting a boundary condition that represented heat and water exchange via the surface of the membrane layer.

### Simulation model of heat and water exchange

Heat is transferred between the air and the organ layer via the membrane layer (supplementary material Fig. S4A). The heat transport of the membrane layer,  $Q_{\text{memb}}$ , from the organ side is determined by Eqn 5. The latent heat,  $Q_{\text{latent}}$ , is calculated from Eqn 6, where  $L$  and  $W_{\text{bl}}$  denote the specific latent heat and water flux from the surface of the membrane layer, respectively.  $L$  is defined by Eqn 7, which was calculated by cubic fitting to the data as reported by Rogers and Yau (1989). The total heat transported,  $Q_{\text{total}}$ , is defined by Eqn 8 as a flux boundary condition for the energy equation (Eqn 3):

$$Q_{\text{memb}} = K_{\text{memb}} \frac{T_S - T_O}{\delta_{\text{memb}}}, \quad (5)$$

$$Q_{\text{latent}} = -LW_{\text{bl}}, \quad (6)$$

$$L = 2500.79 - 0.00000614342 \times T_S^3 + 0.00158927 \times T_S^2 - 2.36418 \times T_S, \quad (7)$$

$$Q_{\text{total}} = Q_{\text{memb}} + Q_{\text{latent}} = K_{\text{memb}} \frac{T_S - T_O}{\delta_{\text{memb}}} - LW_{\text{bl}}, \quad (8)$$

where  $T_S$ ,  $T_O$ ,  $K_{\text{memb}}$  and  $\delta_{\text{memb}}$  denote the temperature of the surface, the organ layer temperature, the thermal conductivity of the membrane layer and the membrane layer thickness, respectively.  $T_O$  is constant, and we set it to  $38.5^\circ\text{C}$ , which is the average body temperature measured in macaques. The thermal conductivity of the mucous membrane,  $K_{\text{memb}}$ , is  $0.6 \text{ W mK}^{-1}$ , which is the thermal conductivity of water (Lervik et al., 2010), because a liquid mucous membrane is assumed in the model used here (Kumahata et al., 2010; Hanida et al., 2013).  $T_S$  is determined by  $Q_{\text{total}}$ , which comprises  $Q_{\text{memb}}$  and  $Q_{\text{latent}}$ .

To simulate water exchange, the wall model was implemented with a boundary layer to define the boundary condition of species transport based on Fick's law (supplementary material Fig. S4B). According to Fick's law, the flux diffusion is proportional to the concentration gradient of water. We used the Dirichlet-type boundary condition, i.e. fixed transport, in FLUENT software. The two-film theory was used to evaluate the mass of species transport between a liquid phase and a gas phase across a boundary. The thickness of the boundary layer was set to 0.5 mm (Hanida et al., 2013).  $W_{\text{bl}}$  is the water flux from the boundary layer, which is determined from Eqn 9, and this was used to calculate the latent heat of Eqns 6 and 8.  $W_{\text{memb}}$  is the water flux from the organ layer, which is determined from Eqn 10.

$$W_{\text{bl}} = D_{\text{bl}} \frac{F - F_S}{\delta_{\text{bl}}}, \quad (9)$$

$$W_{\text{memb}} = D_{\text{memb}} \frac{F_S - F_O}{\delta_{\text{memb}}}, \quad (10)$$

where  $F$ ,  $F_S$ ,  $F_O$ ,  $\delta_{\text{bl}}$ ,  $\delta_{\text{memb}}$ ,  $D_{\text{bl}}$  and  $D_{\text{memb}}$  denote the water fraction in the boundary layer, the water fraction on the membrane surface, the water fraction on the organ layer, the boundary layer thickness, the membrane layer thickness, the mass diffusion coefficient of the boundary layer and the mass diffusion coefficient of the membrane layer, respectively.  $D_{\text{bl}}$  and  $D_{\text{memb}}$  are  $3.0 \times 10^{-5} \text{ m}^2 \text{ s}^{-1}$  and  $2.6 \times 10^{-5} \text{ m}^2 \text{ s}^{-1}$ , respectively (Lee and Wilke, 1954).  $F_O$  is 4.29% of MF with 100% RH at  $38.5^\circ\text{C}$ . It should be noted that diffusion in the boundary layer is greater than that in the membrane layer (Kumahata et al., 2010; Hanida et al., 2013). The water flux is transported from the organ through the membrane and boundary layers to the air. Simultaneously solving Eqns 9 and 10 for  $F_S$  gives Eqn 11. The temperature is not dominant in Eqns 9–11, and the water transport is not regarded as being dependent on temperature in this model. To enable the mass flux of species transport,  $F_S$  was fixed as the boundary condition for water exchange. This boundary condition was implemented

as a user-defined function in FLUENT software:

$$F_S = \frac{\left(\frac{D_{\text{memb}}}{\delta_{\text{memb}}}\right)F_O - \left(\frac{D_{\text{bl}}}{\delta_{\text{bl}}}\right)F}{\left(\frac{D_{\text{memb}}}{\delta_{\text{memb}}}\right) + \left(\frac{D_{\text{bl}}}{\delta_{\text{bl}}}\right)}. \quad (11)$$

### Calculation conditions

The external nostril was modeled as a free inlet, and no-slip boundary conditions were applied at the walls, while the outward velocity was assigned at the pharynx.

The time-averaged speed of inhaled air was calculated based on estimates of the resting tidal volume and the respiratory rate, as well as the measured cross-sectional area of the pharyngeal region at a given position for each subject (supplementary material Table S1). The cross-sectional area was calculated at a given location in the pharynx based on the CT scans using Magics software.

The resting tidal volume was estimated using Eqn 12 (Worthington et al., 1991):

$$TV = 7.69M^{1.04}, \quad (12)$$

where TV and  $M$  are the estimates of the resting tidal volume (ml) and the measured body mass (kg), respectively.

The resting respiratory rate was estimated using Eqn 13 (Stahl, 1967):

$$f = 0.84M^{-0.26}, \quad (13)$$

where  $f$  denotes the estimated respiratory rate (breaths s<sup>-1</sup>).

Finally, the time-averaged speed was calculated using Eqn 14:

$$FV = \frac{2f \times TV}{CA}, \quad (14)$$

where FV and CA denote the time-averaged flow velocity (m s<sup>-1</sup>) and the measured cross-sectional area at a given location in the pharyngeal region (mm<sup>2</sup>), respectively.

The CFD simulations were performed in three ambient atmospheric air conditions: cold-dry, 5°C and 10% RH (0.05% MF); hot-dry, 40°C and 5% RH (0.23% MF); and warm-wet, 30°C and 90% RH (2.38% MF).

### Visualizations

The resulting spatial pattern of the vector quantity representing the velocity and direction of the airflow is illustrated using streamlines in different colors, computed from the points on the plane of the external nostrils (Kumahata et al., 2010; Hanida et al., 2013). The resulting spatial pattern of the scalar quantity representing the temperature and water vapor volume are illustrated using contours in different colors (Kumahata et al., 2010; Hanida et al., 2013).

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### Competing interests

The authors declare no competing or financial interests.

### Author contributions

T.D.N., F.M. and T.M. designed the research; T.D.N., T.M.-N. and J.S. scanned macaques; F.M., S.H., K.K. and T.M. carried out the CFD simulations; T.D.N., F.M., S.H. and T.M. discussed the results; and T.D.N. and F.M. wrote the paper.

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### Supplementary material

Supplementary material available online at <http://jeb.biologists.org/lookup/suppl/doi:10.1242/jeb.118059/-DC1>

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