

HUMAN DEVELOPMENT

RESEARCH REPORT

Three-dimensional cardiac microtissues composed of cardiomyocytes and endothelial cells co-differentiated from human pluripotent stem cells

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ABSTRACT

Cardiomyocytes and endothelial cells in the heart are in close proximity and in constant dialogue. Endothelium regulates the size of the heart, supplies oxygen to the myocardium and secretes factors that support cardiomyocyte function. Robust and predictive cardiac disease models that faithfully recapitulate native human physiology in vitro would therefore ideally incorporate this cardiomyocyteendothelium crosstalk. Here, we have generated and characterized human cardiac microtissues in vitro that integrate both cell types in complex 3D structures. We established conditions for simultaneous differentiation of cardiomyocytes and endothelial cells from human pluripotent stem cells following initial cardiac mesoderm induction. The endothelial cells expressed cardiac markers that were also present in primary cardiac microvasculature, suggesting cardiac endothelium identity. These cell populations were further enriched based on surface markers expression, then recombined allowing development of beating 3D structures termed cardiac microtissues. This in vitro model was robustly reproducible in both embryonic and induced pluripotent stem cells. It thus represents an advanced human stem cell-based platform for cardiovascular disease modelling and testing of relevant drugs.

KEY WORDS: Cardiac microtissue (MT), Human pluripotent stem cell-derived endothelial cells, Human pluripotent stem cell-derived cardiomyocytes, Mesoderm induction, Three-dimensional culture model

INTRODUCTION

Differentiation of human pluripotent stem cells (hPSCs) towards the cardiac lineage offers great potential for studying human heart development in vitro and for developing complex models cardiovascular diseases. Furthermore, hPSC-derived cardiomyocytes have been widely used as platform for developing cardiovascular toxicity tests in vitro (Abassi et al., 2012; Caspi et al., 2009; Guo et al., 2011; Pointon et al., 2013; Rolletschek, 2004; Zeevi-Levin et al., 2012). However, multiple cell types are required

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to build physiologically relevant tissues in vivo and drug-induced cardiotoxicity can have a multicellular component (Cross et al., 2015). For the heart, this means that crosstalk between diverse cell populations, such as the one between cardiac myocytes and endothelial cells of the myocardial vasculature, needs to be captured in a truly representative model (Tirziu et al., 2010).

In development, both cardiomyocytes and endothelial cells originate from lateral plate mesoderm (Garry and Olson, 2006; Moretti et al., 2006). After they form, they communicate via a variety of paracrine, autocrine and endocrine factors. Cardiac endothelium regulates cardiomyocyte metabolism, survival and contractile functions (Brutsaert, 2003; Narmoneva et al., 2004), as well as the delivery of oxygen and free fatty acids to cardiomyocytes (Aird, 2007). Faithful recapitulation of the cardiac tissue environment not only requires consideration of dynamic factors, such as motion and stretch, and electrical communication, but also paracrine signals derived from myocardial endothelial cells (Ravenscroft et al., 2016).

Under physiological conditions, cells are part of a versatile and dynamic network that cannot be recapitulated entirely in twodimensional (2D) monolayer culture (Abbott, 2003). In this regard, scaffold-free tissue-engineering approaches offer unique opportunities for developing three-dimensional (3D) models of the heart muscle in a microtissue (MT) structure. In this format, cardiomyocytes can be seeded alone or in combination with other cardiac cell types, allowing cell aggregation and subsequent tissue formation, and mimicking the native physiological state (Fennema et al., 2013).

The ability of endothelial cells to enhance maturity and pharmacological function of both primary and hPSC-derived cardiomyocytes has been shown in several cardiac tissue models derived from hanging drop cultures, hydrogels, cell sheets and patches (Caspi et al., 2007; Masumoto et al., 2016; Narmoneva et al., 2004; Ravenscroft et al., 2016; Stevens et al., 2009; Tulloch et al., 2011). However, the majority of these approaches used primary cells derived from either human- or non-human sources, as well as non-cardiac-specific endothelial cell types. How endothelial cells, specifically those of the heart, affect hPSC-cardiomyocyte maturation has not been investigated in depth.

Here, we developed a method that allows MTs to form from cardiomyocytes derived from both human embryonic stem cells (hESCs) and human induced pluripotent stem cells (hiPSCs) cultured alone (MT-CM) or in combination with human stem cellderived endothelial cells generated from the same cardiac mesoderm (MT-CMEC). This co-differentiation approach yielded endothelial cells with a cardiac identity. To improve robustness and reproducibility of the system, cell populations were enriched before MT formation and recombined in different ratios. After 7

to 20 days in culture, further evidence of maturity, specifically for MT-CMEC, was shown with increased expression of cardiac genes encoding ion channels and Ca²⁺-handling proteins. In addition, microtissues showed a human dose-response to β -adrenoceptor stimulation, responded to increasing stimulation frequency and displayed negative inotropy after treatment with the Ca²⁺-channel blocker verapamil.

Collectively, our data show the potential of this microtissue model for studying human heart development *in vitro* and for developing complex models of cardiovascular diseases in which either cardiomyocytes or endothelial cells are affected.

RESULTS AND DISCUSSION

Human pluripotent stem cells can be simultaneously differentiated into cardiomyocytes and endothelial cells from cardiac mesoderm

In order to develop an efficient protocol for the simultaneous differentiation of hPSCs into cardiomyocytes and endothelial cells from cardiac mesoderm, we used the NKX2.5eGFP/w hESC line in which enhanced green fluorescent protein (eGFP) is targeted to the genomic locus of the cardiac transcription factor NKX2.5 (Elliott et al., 2011). This allows the appearance and enrichment of cardiomyocytes to be monitored using eGFP expression. Cardiac mesoderm was induced in monolayer culture using a combination of bone morphogenetic protein 4 (BMP4, 20 ng/ml), activin A (20 ng/ ml) and a small-molecule inhibitor of glycogen synthase kinase-3β (CHIR 99021, 1.5 µM) on days 0-3, followed by inhibition of WNT signalling with XAV939 (5 μM) on days 3-6 (Elliott et al., 2011; van den Berg et al., 2016). On day 3 of differentiation, three distinct conditions were tested: (1) differentiation towards cardiomyocyte cell fate (XAV939 from days 3-6 or CM condition); (2) differentiation towards endothelial cell fate (VEGF from days 3-6 or EC condition); and (3) simultaneous differentiation towards endothelial and cardiomyocyte cell fates (XAV939+VEGF from days 3-6 or CMEC condition) (Fig. 1A). Differentiating cell populations were then refreshed on days 6 and 9 with either growth factor-free (CM) or VEGF supplemented (EC and CMEC) medium. Visual assessment of contracting areas (Fig. 1B; Movies 1 and 2) and fluorescence-activated cell sorting (FACS) (Fig. 1C) on day 10 of differentiation revealed that inhibition of WNT signalling was required to form contracting network-like structures, which were composed of $\sim 80\%$ and $\sim 50\%$ eGFP⁺ cardiomyocytes in CM and CMEC conditions, respectively. VEGF was required for endothelial cell specification, resulting in ~16% eGFP-CD31⁺ endothelial cells in EC and CMEC conditions (Fig. 1C). These results demonstrated that inhibition of WNT signalling or VEGF supplementation did not affect endothelial cell or cardiomyocyte formation, respectively. Moreover, VEGF supplementation in the CMEC condition promoted endothelial cell formation at the expense of cardiomyocyte differentiation.

We next performed a time-course experiment to compare the expression of cardiac mesoderm and cardiac-specific genes (MESP1, ISL1, TBX5, NKX2.5 and TNNT2) in CM and CMEC conditions (Fig. 1D). Importantly, expression of these genes started simultaneously in the two groups and followed a similar pattern: MESP1 peaked on day 3, followed by ISL1 and TBX5 induction on days 3 and 5, respectively; NKX2.5 and TNNT2 expression was observed from day 8 onwards. As expected, higher expression of NKX2.5 and TNNT2 was observed in the CM condition compared with CMEC, confirming the FACS data. ETV2, a master regulator of endothelial cell specification, was induced only in the CMEC condition and reached a peak 24 h after VEGF was first added,

confirming previous reports that *ETV2* is activated by VEGF (Orlova et al., 2014; Rasmussen et al., 2012) (Fig. 1D).

Expression of key genes encoding ion channels involved in the generation of the cardiac action potential (AP), such as *CACNA1C*, *SCN5A*, *KCNQ1*, *KCNH2*, *KCNJ12* and *HCN4*, as well as genes encoding Ca²⁺-handling proteins (*SERCA2A* and *NCXI*, also known as *ATP2A2* and *SLC8A1*, respectively) started to appear around day 8 and increased over the time until day 21 (Fig. 1E). No significant differences in gene expression were observed between cardiomyocytes derived under CM or CMEC conditions.

In addition, to characterize the electrical phenotype of these cardiomyocytes, we measured the AP of dissociated cells on day 21 using patch-clamp electrophysiology (Fig. 1F,G; Fig. S1). Representative APs elicited at 1, 2 and 3 Hz are shown in Fig. 1F; AP duration (APD), AP amplitude (APA) and diastolic membrane potential ($E_{\rm diast}$) did not differ between the two groups (Fig. 1G; Fig. S1), suggesting that electrophysiological properties of cardiomyocytes generated in CM and CMEC conditions were comparable.

Using the hESC pre-cardiac MESP1 reporter line (Den Hartogh et al., 2014), we have previously demonstrated that *MESP1*^{mCherry+} progenitors can be differentiated into cardiomyocytes, endothelial cells and smooth muscle cells. Time-course analysis confirmed induction of early cardiovascular progenitor markers (*MESP1*, *TBX5* and *ISL1*) in our present differentiation protocol. Therefore, VEGF supplementation from day 3 causes endothelial cells induced from MESP1⁺ISL1⁺ cardiovascular progenitors to be directed specifically to a cardiac endothelial cell fate. We further demonstrated that VEGF supplementation did not affect cardiomyocyte specification and function, as shown by cardiac ion-channel expression and electrophysiological properties. Collectively, our data demonstrated that both cardiomyocytes and endothelial cells can be differentiated simultaneously from early cardiac mesoderm.

Characterization of CD34⁺ hPSC-derived endothelial cells isolated from cardiac mesoderm

To develop a reliable 3D model of cardiac tissue, we aimed to isolate cardiac endothelial cells derived as above from the heterogeneous differentiated hPSC cultures and mix these with cardiomyocytes in defined ratios. Because CD34, together with VE-cadherin (VEC), is one of the earliest markers of endothelial cell progenitors (Choi et al., 2012; Lian et al., 2014; Orlova et al., 2014), we first performed a time-course experiment to identify optimal differentiation conditions, timing and cell-seeding density for the induction of CD34⁺ endothelial cells (Fig. S2A). Notably, the highest percentage of endothelial cells was observed on day 6 of differentiation in the CMEC condition, by seeding 12.5×10^3 cells per cm². Based on these findings, we isolated CMEC-derived endothelial cells on day 6, using a simple procedure of immunomagnetic selection with anti-CD34 antibody-coupled magnetic beads (Lian et al., 2014). To test whether the same protocol could be applied to hiPSC, we used both NKX2.5eGFP/w hESC and wild-type hiPSC described previously (Zhang et al., 2014).

To determine the extent of CD34⁺ endothelial cell enrichment after isolation, we performed FACS analysis on the cell suspensions before and after purification (Fig. 2A,B). Significant enrichment with >95% CD34⁺ endothelial cell purity was achieved in the postisolation fraction. When subsequently plated, the isolated CD34⁺ cells were highly proliferative, reached confluence within 3 or 4 days and displayed typical endothelial morphology (Fig. 2C). Moreover,

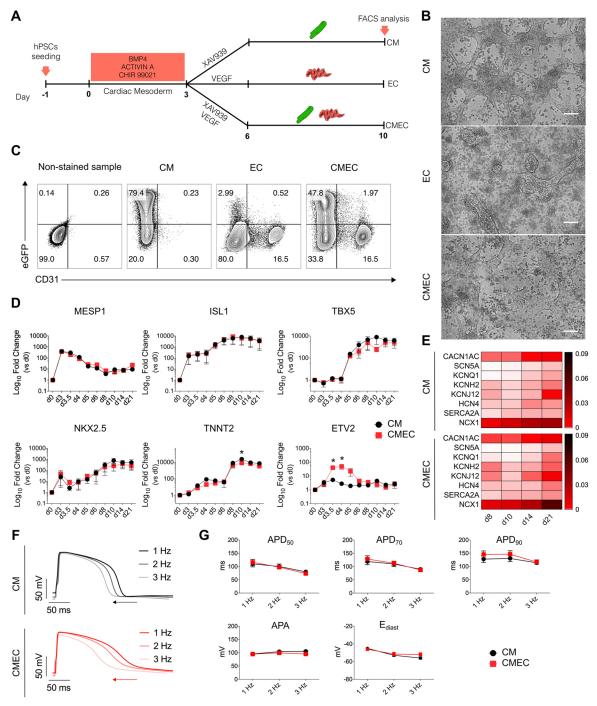


Fig. 1. Simultaneous induction of cardiomyocytes and endothelial cells from cardiac mesoderm. (A) The differentiation protocol towards cardiomyocyte and endothelial cell fates. Cardiac mesoderm was induced with BMP4, activin A and CHIR 99021 from day 0 to day 3, followed by treatment with XAV939 (CM), VEGF (EC) or XAV939+VEGF (CMEC). (B) Bright-field images of day 10 differentiated *NKX2-5*^{eGFP/w} hESCs under CM, EC and CMEC conditions. Scale bars: 100 μm. (C) Representative FACS plots for CD31 together with eGFP of CM, EC and CMEC populations measured in *NKX2-5*^{eGFP/w} hESCs on day 10 of differentiation. Numbers in the quadrants represent the respective percentage of cells. *n*=4. (D) qRT-PCR analysis at the indicated time points (d=day) for selected cardiac genes under CM (black) and CMEC (red) conditions. Values are normalized to *RPL37A* and relative to undifferentiated NKX2.5^{eGFP/w} hESCs. Two-way ANOVA with Sidak's multiple comparisons test. **P*<0.05. *n*=3. Data are mean±s.e.m. (E) Heatmap showing qRT-PCR analysis of key genes encoding ion channels involved in AP shaping and Ca²⁺-handling proteins (linear scale). Values are normalized to *RPL37A* and *TNNT2*, and are relative to undifferentiated NKX2.5^{eGFP/w} hESCs. (F,G) Representative AP traces at 1, 2 and 3 Hz (F), and AP parameter quantification of day 21 *NKX2-5*^{eGFP/w} hESC cardiomyocytes differentiated under CM (black) and CMEC (red) conditions (G). Two-way ANOVA with Sidak's multiple comparisons test. Data are mean±s.e.m. *n*=16-24 from three independent differentiations each.

FACS analysis revealed expression of key endothelial cell-surface markers, such as KDR, VEC, CD34 and CD31, in both hESC- and hiPSC-derived CD34⁺ endothelial cells (Fig. 2D). Notably, these

cells were also positive for the arterial marker CXCR4. At this stage, endothelial cells were suitable for either MT formation or, alternatively, cryopreservation for later use (Fig. S2B).

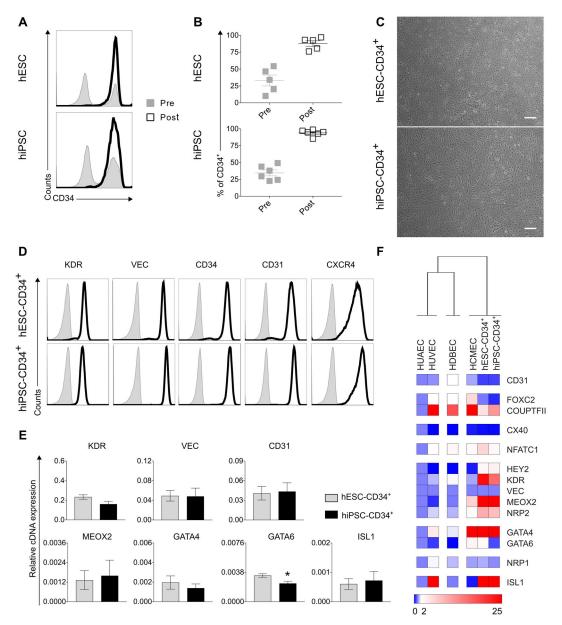


Fig. 2. Isolation and characterization of endothelial cells. (A,B) FACS histograms from representative experiments (A) and averaged percentages from multiple experiments (B) of CD34⁺ cells in the pre-isolation (grey) and post-isolation (black) fractions showing the efficiency of the isolation strategy. Experiments were performed on cells derived from *NKX2-5*^{eGFP/w} hESCs (upper panels, *n*=5) and hiPSCs (lower panels, *n*=6). (C) Representative bright-field images of the morphological appearance of CMEC-derived CD34⁺ cells from *NKX2-5*^{eGFP/w} hESCs (upper panel) and hiPSCs (lower panel) after isolation and re-plating. Scale bars: 200 μm. (D) FACS measurement (histograms) for key endothelial cell-surface markers of CD34⁺ cells 4 days after isolation and re-plating. Specific antibody-labelled cells are shown in black (*NKX2-5*^{eGFP/w} hESC line, upper panels; hiPSC line, lower panels) (*n*=3). (E) qRT-PCR analysis for key endothelial genes (upper panels) and for cardiac-specific genes (lower panels) in CMEC-derived CD34⁺ cells from *NKX2-5*^{eGFP/w} hESCs (grey) and hiPSCs (black). Mann–Whitney test. **P*=0.0286. *n*>3. Data are mean±s.e.m. Values are normalized to *RPL37A*. (F) qRT-PCR analysis (heatmap) and hierarchical clustering showing a panel of endothelial and cardiac genes of interest in HUAECs, HUVECs, HDBECs and HCMECs together with CMEC-derived CD34⁺ cells from NKX2.5^{eGFP/w} hESCs and hiPSCs (*n*=3). Values are normalized to *RPL37A* and *VEC*, and are relative to HUAECs.

To characterize endothelial cells isolated on day 6, we determined the expression of typical endothelial markers such as *KDR*, *VEC* and *CD31*, as well as cardiac-specific markers, such as *MEOX2*, *GATA4*, *GATA6* and *ISL1*, by quantitative RT-PCR (qRT-PCR) (Fig. 2E). These day 6 CD34⁺ endothelial cells derived from both hESC and hiPSC exhibited comparable marker expression. Moreover, when compared with primary endothelial cells such as human umbilical artery endothelial cells (HUAECs), human umbilical vein endothelial cells (HUVECs), human dermal blood endothelial cells (HDBECs) and human cardiac microvascular endothelial cells

(HCMECs), day 6 CD34⁺ endothelial cells clustered with HCMEC and showed similar expression of the cardiac-specific marker *GATA4* (Fig. 2F). This is consistent with previously reported data demonstrating that *GATA4* is crucial for heart formation during embryonic development and strongly implicated in congenital heart diseases (Butler et al., 2010; Furtado et al., 2016; Garg et al., 2003), and suggests a cardiac endothelium identity for the CMEC-derived endothelial cells.

Endothelial cells can differentiate from different types of mesoderm. In the heart, they originate from both endocardial and

second heart-field progenitors (Misfeldt et al., 2009; Sahara et al., 2015). Importantly, in the developing postnatal mouse heart, endocardium contributes to more than 70% of coronary endothelium (Espinosa-Medina et al., 2014; Tian et al., 2015). Although very little is known about the developmental and the genetic signature of human endocardial (endothelial) cells, lineage tracing has demonstrated that these cells originate from both multipotent cardiac progenitors and early cardiac mesoderm (Misfeldt et al., 2009). We therefore investigated whether we could differentiate endothelial cells from a common cardiac mesoderm. Interestingly, we found that day 6 endothelial progenitors exhibited a similar genetic signature to human primary cardiac endothelial cells (Fig. 2F). Most strikingly, increased expression of MEOX2, GATA4, GATA6 and ISL1 was observed compared with primary non-cardiac endothelial cells. Future genome-wide transcriptional studies will be required for in depth characterization of the cardiac/endocardial origin of these endothelial cells. Other stimuli, such as the upregulation of fatty acid transporters, could help to determine whether co-culture with cardiomyocytes can shift their cardiac endothelial cell profile closer to bona fide cardiac endothelial cells (Coppiello et al., 2015; Hagberg et al., 2013; Jang et al., 2016).

hPSC-VCAM1-enriched cardiomyocytes display typical sarcomeric structures and cardiac electrophysiological properties

In order to obtain a defined cardiomyocyte population, we used VCAM1, previously described as a cardiomyocyte surface marker, to isolate VCAM1⁺ cells from differentiated cultures (Skelton et al., 2014; Uosaki et al., 2011; Wang et al., 2014). As with the endothelial purification strategy, we first performed time-course analysis using NKX2.5eGFP/w hESC to identify optimal differentiation conditions, timing and cell-seeding density for the differentiation of VCAM1⁺ cardiomyocytes in CM and CMEC conditions (Fig. S3A). Cells from both conditions showed initial expression of VCAM1 at day 10, reaching a maximum on day 14, in agreement with previous studies on hESC differentiation (Skelton et al., 2014). The CM condition resulted in higher numbers of eGFP+VCAM1+ cells compared with the CMEC condition. Moreover, the highest percentage of cardiomyocytes was observed by seeding 25×10³ cells per cm². Using these conditions for both NKX2.5eGFP/w hESC and the wild-type hiPSC, VCAM1+ cells were enriched by immunomagnetic selection with anti-VCAM1-PE-labelled antibody-coupled magnetic beads. FACS analysis on cell suspensions before and after isolation revealed ~80% enrichment of VCAM1⁺ cells (Fig. 3A,B). Importantly, after bead sorting, VCAM1⁺ cells re-plated in culture re-formed spontaneously contracting networks within 3-4 days (Fig. S3B; Movie 3), accompanied by NKX2.5-eGFP expression in the hESC line (Fig. S3C). Furthermore, VCAM1+ cells displayed characteristic sarcomeric structures that stained positively for troponin I (TNNI) and α -actinin (Fig. 3C).

Electrophysiological properties of VCAM1⁺ cardiomyocytes were next compared with non-enriched cardiomyocytes (Fig. 3D, E; Fig. S3D). Current clamp measurements revealed no significant differences between the two groups in the NKX2.5^{eGFP/w} hESC line (Fig. 3D,E; Fig. S3D). In the hiPSC line, although VCAM1⁺ cells displayed shorter APD₅₀ and APD₇₀ at 1 and 2 Hz, they did not show significant differences in APD₉₀, APA and E_{diast} when compared with the non-enriched population (Fig. 3D,E; Fig. S3D).

Enrichment of the cardiac population from differentiated cultures based on VCAM1 expression has been previously described (Elliott et al., 2011; Schwach and Passier, 2016; Skelton et al., 2014; Uosaki et al., 2011; Wang et al., 2014), but the electrical phenotype of purified cardiomyocytes had not been assessed to date. Here, we optimised a protocol based on anti-PE magnetic nanoparticles, which allowed isolation of VCAM1⁺ cardiomyocytes with high viability, and supported maintenance of their typical sarcomeric structure and electrophysiological properties ready for downstream applications.

hPSC-derived endothelial cells and cardiomyocytes form 3D contracting cardiac microtissues

To optimize conditions for generating cardiac MTs, we first used either non-enriched or VCAM1-enriched hESC-cardiomyocytes either alone (MT-CM) or in combination with hESC-derived CD34⁺ endothelial cells (MT-CMEC). Spheroid MTs were formed in V-bottomed 96-well microplates and were refreshed every 3 days with either growth factor-free (MT-CM) or VEGF-supplemented (MT-CMEC) medium. MTs were characterized between days 7 and 20 after initial aggregation (Fig. 4A).

To determine the morphology and the cellular architecture of both MT-CM and MT-CMEC, we performed immunostaining for cardiomyocyte- and endothelial-specific cell markers (using TNNI and CD31 antibodies, respectively). In addition, to define optimal endothelium/myocyte ratios within the MTs, different percentages of cardiomyocytes and CD34⁺ cells were combined (Fig. 4B; Fig. S4A). Interestingly, immunohistochemistry revealed that MTs composed of 15% endothelial cells and 85% cardiomyocytes resulted in a better endothelial cell organization and distribution within the MT compared with MTs containing 40% endothelial cells (Fig. S4A). After optimizing conditions for MT formation using hESCs, we used the same protocol for wild-type hiPSCs. Immunofluorescence analysis confirmed TNNI and CD31 expression in 3D MTs generated from VCAM1⁺ cardiomyocytes in combination with 15% CD34⁺ endothelial cells (Fig. 4C). Importantly, VCAM1+ bead-sorted cardiomyocytes maintained their ability to form 3D aggregates alone or in combination with endothelial cells.

Next, to investigate whether gene expression was changed by 3D organization and/or the presence of endothelial cells, we compared expression of a broad panel of genes in MT-CM and MT-CMEC with 2D monolayer VCAM1+ cardiomyocytes by qRT-PCR. Specifically, we quantified expression of genes involved in sarcomere assembly (MYL2, MYL7, MYL4, MYL3, MYH6, MYH7, TNN11, TNN13, ACTN2, TCAP and ACTA1), in cardiac AP (SCN5A, CACNA1C, KCNQ1, KCNE1, KCNH2, KCNJ12, KCNJ2 and HCN4) and in Ca²⁺ handling (NCX1, SERCA2A, PLN, RYR2, CASQ2, S100A1 and TRDN). In addition, expression of fetal cardiomyocyte-enriched genes (NPPA and NPPB), as well as the sarcomeric mitochondrial gene CKMT2 (Babiarz et al., 2012; Chun et al., 2015; Payne and Strauss, 1994) and the $\alpha 7$ integrin subunit (ITGA7), were also quantified (Fig. 4D; Fig. S4B).

After 7 days in culture, MT-CMEC showed gene expression changes associated with progression of heart development and fetal-to-postnatal transition: upregulation of the sarcomeric structural genes TNNT2, MYL2, ACTN2 and TCAP; upregulation of the ion-channel genes SCN5A, CACNA1C, KCNJ12 and KCNJ2; upregulation of the Ca²⁺-handling genes SERCA2A, RYR2 and TRDN; upregulation of CKMT2 and ITGA; and downregulation of the fetal-enriched gene NPPB. Conversely, changes in other genes not associated with advanced maturation were also observed: upregulation of the fetal sarcomeric structural genes MYH6 and TNNII; upregulation of HCN4; and downregulation of the adult

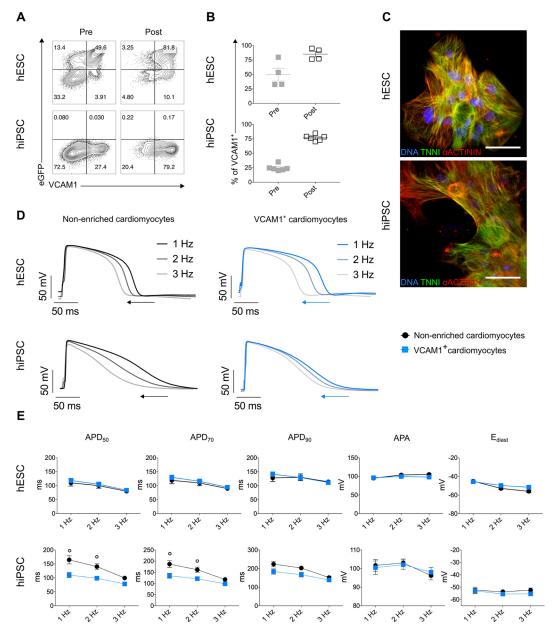


Fig. 3. Isolation and characterization of cardiomyocytes. (A,B) FACS plots from representative experiments analysing VCAM1 and eGFP (A), and average percentages from multiple experiments of VCAM1⁺ cells (B) in the pre-isolation (grey) and post-isolation (black) fractions showing the efficiency of the isolation strategy. Experiments were performed on cells differentiated from *NKX2-5*eGFP/w hESCs (upper panels, *n*=4) and hiPSCs (lower panels, *n*=6). (C) Immunofluorescence images of cardiac sarcomeric proteins TNNI (green) and α-actinin (red) in VCAM1⁺ cardiomyocytes generated from NKX2.5eGFP/w hESCs (upper panel) and hiPSCs (lower panel). Nuclei are stained in blue with DAPI. Scale bars: 50 μm. (D,E) Representative APs at 1, 2 and 3 Hz (D), and AP parameter quantification of non-enriched (black) and VCAM1⁺ (blue) cardiomyocytes differentiated from *NKX2-5*eGFP/w hESCs (upper panels, *n*=16 and 16) and hiPSCs (lower panels, *n*=15 and 18) from three independent differentiations each (E). Two-way ANOVA with Sidak's multiple comparisons test. *P*<0.05 versus VCAM1⁺ cardiomyocytes. Data are mean±s.e.m.

sarcomeric structural gene *TNNI3*. A similar trend for the majority of genes was observed in MTs generated from hESCs, although not all changes were consistent with hiPSC-MTs (Fig. S4B).

Furthermore, to investigate whether maturation increased with time in culture, we generated MTs from both hESCs and hiPSCs, and cultured them for 20 days (Fig. S5). Gene expression analysis at this time point showed upregulation of cardiac ion-channel genes (SCN5A, CACNA1C, KCNQ1 and KCNE1), upregulation of the Ca²⁺-handling genes CASQ2 and TRDN as well as downregulation of the foetal cardiomyocyte-enriched genes MYH6 and TNNI1 (Fig. S5A,B). In addition, day 20 MTs from both hESCs and

hiPSCs displayed increased MYL2/MYL7 and MYH7/MYH6 ratios when compared with day 7 MTs (Fig. S5C,D).

Taken together, our results suggested that 3D culture organization, inclusion of endothelial cells and prolonged time in culture induced crucial changes in the gene expression of cardiomyocytes that were associated with maturation in our *in vitro* cardiac microtissue system.

Next, to investigate the electrical phenotype of MT-CM and MT-CMEC, we measured QT and RR intervals using multielectrode array (MEA) at baseline and following addition of increasing concentrations of the β -adrenoreceptor agonist

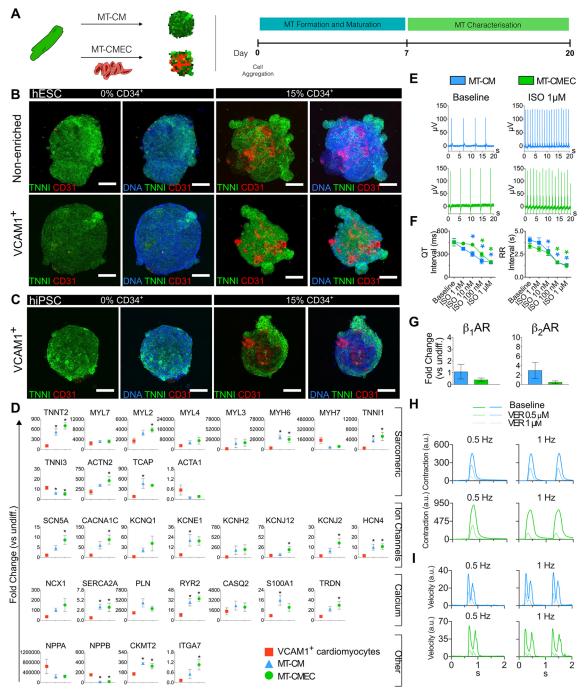


Fig. 4. Generation and characterization of 3D cardiac microtissues. (A) The protocol to generate cardiac MTs from cardiomyocytes cultured alone (MT-CM) or in combination with enriched CD34⁺ endothelial cells (MT-CMEC). MTs from NKX2-5^{eGFP/w} hESCs were generated from non-enriched or enriched VCAM1⁺ cardiomyocytes, whereas MTs from hiPSCs were generated from enriched VCAM1+ cardiomyocytes only. MT characterization was performed between days 7 and 20 by immunofluorescence, qRT-PCR, MEAs and contraction analyses. (B) Immunofluorescence analysis of sarcomeric cardiac TNNI (green) and endothelial cell surface marker CD31 (red) of day 7 cardiac MTs from non-enriched (upper panels) and VCAM1-enriched (lower panels) cardiomyocytes from NKX2-5eGFP/w hESCs. Percentages of CD34+ cells are shown at the top. Scale bars: 100 µm. (C) Immunofluorescence analyses of TNNI (green) and CD31 (red) of day 7 MTs generated from hiPSC-VCAM1+ cardiomyocytes. Percentages of CD34+ cells are shown at the top. Scale bars: 100 µm. (D) qRT-PCR analysis for key sarcomeric genes, ion channels involved in AP shaping and Ca²⁺ regulatory genes, as well as other cardiac genes of interest in day 7 hiPSC-MTs and in day 21 age-matched VCAM1⁺ cardiomyocytes from hiPSCs. All values are normalized to RPL37A and relative to undifferentiated hiPSCs. Data are mean±s.e.m., n>4. One-way ANOVA with Tukey's multiple comparisons test. *P<0.05 versus VCAM1* cardiomyocytes. (E) FP representative traces measured using MEAs under baseline conditions (left panels) and upon addition of 1 µM isoprenaline (ISO) (right panels) in MT-CM (upper panels, blue) and MT-CMEC (lower panels, green) from hiPSCs. (F) QT and RR intervals measured using MEAs under baseline conditions and after increasing concentrations of ISO in MT-CM (blue) and MT-CMEC (red) from hiPSCs. One-way ANOVA. *P<0.05 versus baseline. Colour code of the asterisks indicates the experimental group. Data are mean±s.e.m., n=9. (G) qRT-PCR analysis of β-adrenoreceptors (β₁ AR, left panel; β₂ AR, right panel) in day 7 MT-CM and MT-CMEC from hiPSCs. Values are normalized to RPL37A and are relative to undifferentiated hiPSCs. Mann-Whitney test. Data are mean±s.e.m., n=3. (H,I) Representative traces of contraction (H) and contraction velocity (I) in MT-CM (blue) and MT-CMEC (green) generated from hiPSCs and paced at 0.5 (left panels) and 1 Hz (right panels). Results are shown under baseline conditions and after superfusion of 500 nM and 1 µM verapamil (VER).

isoprenaline (ISO) (Fig. 4E,F; Fig. S6). Representative field potential (FP) recordings at baseline and after addition of 1 μ M ISO are shown in Fig. 4E. Interestingly, QT and RR intervals did not differ between the MT-CM and MT-CMEC groups (Fig. 4F), and the dependence of QT interval duration from the RR interval was uniform in the two groups (Fig. S6), suggesting that the baseline electrical properties of the MT were conserved with or without endothelial cells. However, in MT-CM, 10 nM ISO significantly shortened QT and RR intervals compared with baseline values, whereas MT-CMEC required a higher concentration of ISO (100 nM) to undergo significant shortening. This might be due to the lower expression of β_1 and β_2 adrenoreceptor genes (*ADRB1* and *ADRB2*, respectively) in MT-CMEC compared with MT-CM, which might be linked to the different cell composition (Fig. 4G; Fig. S7A).

Finally, qualitative analysis of MT contraction was performed in paced hiPSC-MTs and in hESC-MTs at 0.5 and 1 Hz (Fig. 4H,I; Fig. S7B,C), under baseline conditions and after treatment with the Ca²⁺-channel blocker verapamil (VER, 500 nM and 1 μ M). Notably, VER decreased the contraction amplitude and velocity, as expected from the block of the L-type Ca²⁺ channels and as observed earlier in MTs with primary endothelial cells (Ravenscroft et al., 2016).

Taken together, we conclude that the in vitro cardiac microtissue that we have developed represents a robust system suitable for medium- to large-scale production and a valid tool for studying cardiomyocyte maturation, disease modelling and drug screening. Importantly, additional studies are required to assess full cardiomyocyte maturation, including sarcomeric organization, mitochondria content, and replication of the physiological and pharmacological responses that are typical of the native human heart tissue. Compared with existing systems (Table S3), ours has both limitations and advantages. For example, compared with engineered heart tissues (EHTs), microtissues required a substantially smaller number of cells and therefore are more amenable to large-scale production. However, EHTs display cell and sarcomeric alignment, and allow the measurement of contractile force; EHTs have been able to recapitulate the positive and negative inotropic effects of molecules and drugs in the heart (Mannhardt et al., 2016). Micro-heart muscles combine the advantages of scalability, cell alignment and force measurement (Huebsch et al., 2016).

Undoubtedly, increasing the complexity of our microtissue format by inclusion of other cardiac cell types and complex 3D architectures, or even by implementation of fluid flow for the endothelial cells has to be explored to further improve the system. In addition, the fact that cardiomyocytes and endothelial cells possess different metabolic states also needs to be taken into account: on the one hand, embryonic or immature cardiomyocytes are highly dependent on glycolysis, whereas maturation is associated with the switch towards fatty acid oxidation; on the other hand, endothelial cells are highly dependent on glycolysis for active angiogenesis (Schoors et al., 2014). Therefore, the correct balance between glucose and free fatty acid supplementation will be essential to promote further maturation in our system. Furthermore, as endothelial cells serve as a semipermeable barrier for the delivery of nutrients to the cardiomyocytes, a separation of either the fluid or the nutrient compartment might be essential to prevent direct contact with cardiomyocytes. Finally, it will be interesting to investigate whether maturation of endothelial cells is also improved in the MT system described here.

MATERIALS AND METHODS

hPSC lines culture and differentiation into endothelial cells and cardiomyocytes

Previously described NKX2-5^{eGFP/w} hESCs and wild-type hiPSCs (Elliott et al., 2011; Zhang et al., 2014) were cultured in E8 medium (Life Technologies). Cardiac and endothelial differentiations were induced in a monolayer: CM condition as previously described (van den Berg et al., 2016; Elliott et al., 2011); details of EC and CMEC conditions are provided above and in the supplementary Materials and Methods.

FACS analysis

Staining was carried out with the following antibodies: anti-VCAM1-PE, anti-CD34-APC, anti-KDR-PE, anti-VEC-PECY7, anti-CD31-APC and anti-CXCR4-PE. Further details are provided in the supplementary Materials and Methods. Antibodies are listed in Table S2.

Isolation of CD34⁺ endothelial cells and VCAM1⁺ cardiomyocytes

CD34⁺ cells were isolated using a Human Cord Blood CD34 Positive Selection kit II (StemCell Technologies) whereas VCAM1⁺ cells were isolated using a Human PE Selection kit (StemCell Technologies) following the manufacturer's instructions (see also supplementary Materials and Methods).

Generation and cultivation of cardiac microtissues

CD34⁺ endothelial cells and enriched or non-enriched VCAM1⁺ cardiomyocytes were prepared prior to microtissue formation and combined for self-aggregation as described in the supplementary Materials and Methods.

Immunofluorescence analysis

Immunostaining was carried out with the following primary antibodies: TNNI and α -actinin for VCAM1 $^+$ cardiomyocytes; and CD31 and TNNI for MTs. Primary antibodies were detected using Cy3- and Alexa Fluor 488-conjugated secondary antibodies. Further details are provided in the supplementary Materials and Methods.

Patch-clamp and multielectrode array electrophysiology

Electrical signals for patch-clamp single cell analysis were recorded with an Axopatch 200B Amplifier (Molecular Devices) and digitized with a Digidata 1440A (Molecular Devices), and MEA experiments were performed using a 64-electrode USB-MEA system (Multichannel Systems) as previously described (Sala et al., 2016). Details are provided in the supplementary Materials and Methods.

Contraction analysis

Movies of paced MTs were acquired with a ThorLabs DCC3240M camera and analysed with a custom-made algorithm. Details are provided in the supplementary Materials and Methods.

Drugs

Isoprenaline (Sigma-Aldrich) was dissolved in MilliQ water and verapamil (Sigma-Aldrich) was dissolved in 100% ethanol following the manufacturer's instructions. Stock solutions were freshly prepared before experiments.

Gene expression analysis

For RT-qPCR, RNA was purified using the RNeasy Mini Kit (Qiagen) and reverse transcribed using the iScript-cDNA Synthesis kit (Bio-Rad). Gene expression was assessed using a Bio-Rad CFX384 real-time system and data were analysed using the $\Delta\Delta Ct$ method. Further details are provided in the supplementary Materials and Methods. Primer sequences can be found in Table S1.

Bright-field images and movies

Bright-field images and movies were acquired with a Nikon DS-2MBW camera connected to a Nikon Eclipse Ti-S microscope controlled by the

Nikon NIS-Element BR software. Lens magnification was $4\times$ or $10\times$ with a PhL or Ph1 contrast filter.

Statistics

Ordinary one-way, two-way ANOVA and Mann–Whitney tests for paired or unpaired measurements were applied for differences in means between groups/conditions. Detailed statistics are indicated in each figure legend. Data are expressed as mean \pm s.e.m. Statistical significance was defined as P<0.05. Further details are provided in the supplementary Materials and Methods.

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Competing interests

C.L.M. is co-founder of Pluriomics.

Author contributions

E.G. carried out cell culture, differentiations and isolations, generated microtissues, performed FACS, qRT-PCR and immunofluorescence analyses, designed the experiments, and wrote the manuscript. M.B. designed the experiments and wrote the manuscript. L.S. performed single cell patch-clamp, MEA electrophysiology, contraction measurements and analysis, designed the experiments, and wrote the manuscript. B.J.v.M. performed contraction measurements and analysis. L.G.J.T. performed contraction measurements and analysis. V.V.O. designed the experiments and wrote the manuscript. C.L.M. designed the experiments and wrote the manuscript.

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Supplementary information

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SUPPLEMENTARY MATERIALS AND METHODS

hPSC lines culture

Previously described NKX2-5^{eGFP/w} hESCs and wild-type hiPSCs (Elliott et al., 2011; Zhang et al., 2014) were seeded on Vitronectin Recombinant Human Protein (Life technologies) and cultured in E8 medium (Life Technologies). Cells were passaged twice a week using PBS (Life Technologies) containing EDTA 0.5mM (Life Technologies). RevitaCell Supplement (Life Technologies; 1:200) was added during hiPSC passaging.

Differentiation into endothelial cells and cardiomyocytes

Cardiac differentiation was induced in a monolayer as described previously (Elliott et al., 2011; van den Berg et al., 2015). Briefly, for CM condition, $25 \times 10^3 / \text{cm}^2$ were seeded on plates coated with 75 µg/mL (growth factor reduced) Matrigel (Corning) the day before differentiation (day -1). At day 0, cardiac mesoderm was induced by changing E8 to BPEL medium (Bovine Serum Albumin [BSA] Polyvinyl alcohol Essential Lipids; (Ng et al., 2008)), supplemented with a mixture of cytokines (20 ng/mL BMP4, R&D Systems; 20 ng/mL ACTIVIN A, Miltenyi Biotec; 1.5 µM GSK3 inhibitor CHIR99021, Axon Medchem). After 3 days, cytokines were removed and a Wnt inhibitor (5 µM, XAV939, Tocris Bioscience) was added for 3 days. BPEL medium was refreshed every 3–4 days. Alternatively, for EC and CMEC conditions, 12.5×10^3 cells/cm² were seeded on matrigel at day -1. At day 0, cardiac mesoderm was induced as described above. At day 3, cytokines were removed and VEGF (50 ng/ml, R&D Systems) alone (EC condition) or in combination with XAV939 (5 µM) (CMEC condition) was added. BPEL medium supplemented with VEGF was refreshed every 3–4 days.

FACS analysis

Staining was done in PBS containing 0.5% BSA (Sigma Aldrich) and 2 mM EDTA. Antibodies were used as follows: anti-VCAM1-PE (R&D); anti-CD34-APC (Miltenyi Biotech), anti-KDR-PE (R&D), anti-VEC-PECY7 (eBioscience), anti-CD31-APC (eBioscience), anti-CXCR4-PE (BD Biosciences); MACS Comp Bead kit antimouse IgK (Miltenyi Biotech). Samples were measured with a MACSQuant VYB (Miltenyi Biotech) equipped with a violet (405 nm), blue (488 nm) and yellow (561 nm) laser. In order to allow direct comparisons between different experimental groups, equal population gates were applied. Details of antibodies used are provided in Supplementary Table S2.

Isolation of CD34⁺ endothelial cells

CMEC population was detached on day 6 using TrypLE 1X for 5 min at 37°C, 5% CO₂, centrifuged for 3 min at 1100 rpm, washed and re-suspended in 1 ml of EasySep buffer (PBS containing 2% FCS [Life Technologies] and 1mM EDTA) into a 5mL round-bottomed tube. Before isolation, a small aliquot was taken for anti-CD34-APC antibody staining and FACS

analysis (pre-isolation fraction). CD34⁺ cells were isolated using a Human cord blood CD34 Positive selection kit II (Stem Cell Technologies) following the manufacturer's instructions. After isolation, an aliquot of post-isolation fraction was taken for anti-CD34-APC antibody staining and FACS analysis. CD34⁺ cells were resuspended in BPEL medium and counted. For CD34⁺ culture, 10 × 10³/cm² cells were seeded on Fibronectin (Fibronectin from bovine plasma 2-5µg/ml; Sigma Aldrich) and cultured in BPEL medium supplemented with VEGF (50ng/ml). After 3-4 days, cells were confluent and cryopreserved (30cm²/vial) in CryoStor[®] CS10 medium (0.5ml/vial; Stem Cell Technologies) or dissociated for MT formation.

Isolation of VCAM1⁺ cardiomyocytes

CM population was detached on day 14-17 using TrypLE 2X for 5 min at 37°C, 5% CO₂, centrifuged for 3 min at 1100 rpm, washed and re-suspended in 1 ml of EasySep buffer into a 5mL round-bottom tube. Cell suspension was stained for 30 min at 4C with an anti-VCAM1-PE antibody described previously. After 30 min, a small aliquot was taken for FACS analysis (pre-isolation fraction). VCAM1⁺ cells were isolated by using a Human PE Selection kit (Stem Cell Technologies) following the manufacturer instructions. After isolation, a small aliquot of post-isolation fraction was taken for FACS analysis. VCAM1⁺ cells were resuspended in BPEL medium, counted and used for electrophysiology, immunofluorescence or MT formation.

Generation and cultivation of cardiac microtissues

To generate MTs from isolated VCAM1⁺ cardiomyocytes, CM population was stained with anti-VCAM1-PE antibody and isolated as described above. Alternatively, CM population was dissociated using TrypLE 2X for 5 min at 37°C, 5% CO₂ (non-enriched VCAM1⁺ cardiomyocytes). Endothelial cells were prepared as follow: briefly, 1 to 3 days before MT formation, a vial of cryopreserved endothelial cells was thawed and cultured in BPEL medium supplemented with VEGF (50 ng/ml) on Fibronectin-coated plates (Fibronectin from bovine plasma 2-5µg/ml; Sigma Aldrich). The day of MT formation (day 0), endothelial cells were detached using TrypLE 1X for 5 min at 37 °C, 5% CO₂, centrifuged for 3 min at 1100 rpm and resuspended in BPEL medium. For MT-CM: cardiomyocytes were diluted to 5000 cells per 50 µl BPEL medium. For MT-CMEC: cell suspensions were combined together to 5000 cells per 50 µl BPEL medium supplemented with 50 ng/ml VEGF. For both MT-CM and MT-CMEC, cell suspensions were seeded on V-bottom 96 well microplates (Greiner bio-one) and centrifuged for 10 min at 1100 rpm. MTs were incubated at 37°C, 5% CO2 for 7-20 days with media refreshed every 3 days. Analysis of MTs was performed after 7-20 days in culture.

Immunofluorescence analysis

For immunostaining of VCAM1 $^+$ cardiomyocytes, approximately 200 × 10 3 /cm 2 cells were seeded on 75 µg/mL Matrigel-coated 13 mm plastic coverslips (Sarstedt) and fixed for 20 min in 4% paraformaldehyde, permeabilized for 10 min with PBS containing 0.1% Triton-X 100 (Sigma-Aldrich) and blocked for 1h with PBS containing 5% (vol/vol) FCS and 5% goat serum

(Vector Laboratories). Samples were incubated overnight at 4° C with TNNI (Santa Cruz) and α -ACTININ (Sigma–Aldrich) antibodies. Primary antibodies were detected with Cy3-(Dianova) and Alexa Fluor 488- (Invitrogen) conjugated donkey secondary antibodies, for 1h at room temperature. Cells were washed three times with PBS, each time incubated for 20 min and stained with DAPI (Life Technologies) for 30 min at room temperature. Stained cells were mounted onto microscope slides with ProLong Gold antifade Mountant with DAPI (Life Technologies). Images were captured using Leica Microsystems LAS AF6000. Details of antibodies used are provided in Supplementary Table S2.

For whole mount microtissue immunofluorescence staining, MTs were washed in PBS on day 7 and fixed for 30 min with 4% paraformaldehyde, washed 3 times in PBS and stored at 4 °C until processing. MTs were permeabilized for 20 min with PBS containing 0.2% Triton X-100 and blocked for 2 h in PBS containing 5% FCS and 5% goat serum. All incubations were done at room temperature. Samples were then incubated overnight at 4°C with CD31 (Dako) and TNNI primary antibodies. MTs were washed 3 times with PBS at room temperature, each time incubated for 10 min. Secondary antibodies (Cy3 and Alexa Fluor 488) were added overnight at 4°C. The following day, MTs were washed 3 times with PBS at room temperature, each time incubated for 20 min and then stained with DAPI for 30 min at room temperature. MTs were mounted onto microscope slides with ProLong Gold antifade Mountant with DAPI. Images were captured using a Leica SP8WLL confocal laser-scanning microscope. Details of antibodies used are provided in Supplementary Table S2.

Patch Clamp

Electrical signals were recorded with an Axopatch 200B Amplifier (Molecular Devices) and digitized with a Digidata 1440A (Molecular Devices) connected to an x86 Windows PC running pClamp 10.4. All measurements were performed at 37 °C. Data were analyzed with ClampFit 10.4 (Molecular Devices) and Prism 7.0a (Graphpad Software) for Mac. Current-clamp experiments were performed in the perforated patch configuration. Cells were perfused with Tyrode's solution containing (mM): 154 NaCl, 5.4 KCl, 1.8 CaCl₂, 1 MgCl₂, 5 HEPES-NaOH, 5.5 D-Glucose; pH was adjusted to 7.35 with NaOH. Glass capillaries (2-3.5 M Ω) were filled with an intracellular solution containing (mM): 125 K-Gluconate, 20 KCl, 10 NaCl, 10 HEPES; pH was adjusted to 7.2 with KOH. Amphotericin B (Sigma Aldrich) was dissolved in DMSO just before the experiments and added to the intracellular solution to reach a final concentration of 0.22 mM.

Multielectrode array (MEA)

MEA experiments were performed using a 64 electrodes USB-MEA system (Multichannel Systems). All the experiments were performed at 37 $^{\circ}$ C in BPEL medium. MEA chambers were coated with human Fibronectin (40 μ g/ml, Alfa Aesar) before MT seeding. Acute doseresponse curves were generated by adding aliquots at fixed 1:100 dilutions every 10 min

(Navarrete et al., 2013). Traces were analyzed with a custom-made protocol to quantify both QT and RR intervals.

Contraction analysis

Movies of paced MTs were acquired with a ThorLabs DCC3240M camera at 100 frames per second with the ThorLabs uc480 software (v 4.20). Contraction and contraction velocity profiles were obtained by analysing movies with a custom-made ImageJ macro (ImageJ v. 2.0.0-rc-49).

Gene expression analysis

For RT–qPCR, total RNA was purified using the RNeasy Mini Kit (Qiagen) according to the manufacturer's protocol. 1 μ g of RNA was reverse transcribed by using the iScript-cDNA Synthesis kit (Bio-Rad). Expression profiles of genes of interest were determined by qPCR using 6ng/ μ l of cDNA and the iTaq Universal SYBR Green Supermixes (Bio-Rad). Gene expression was assessed by a Bio-Rad CFX384 real time system. The expression of two reference genes (*RPL37A* and *HARP*) was stable in our samples and not affected by experimental conditions, therefore only *RPL37A* was used for normalization. Data were analyzed by using the $\Delta\Delta$ Ct method (Livak and Schmittgen, 2001; Pfaffl, 2001). Further normalization to TNNT2 or *VEC* is specified in figure legends. Primer sequences are provided in Supplementary Table S1.

Cell pellets of primary Human Umbilical Artery Endothelial Cell (HUAEC), Human Umbilical Vein Endothelial Cell (HUVEC), Human Dermal Blood Endothelial Cell (HDBEC) and Human Cardiac Microvascular Endothelial Cell (HCMEC) from PromoCell were used to extract RNA as described above.

Statistics

Ordinary one-way, two-way ANOVA or Mann-Whitney test for paired or unpaired measurements were applied as appropriate to test for differences in means between groups/conditions. Post hoc comparison between individual means or medians was performed by Tukey's method, and P-values have been corrected for multiple testing using the Holm–Sidak or Dunn's method. Detailed statistics are indicated in each figure legend. Data are expressed and plotted as the Mean ± SEM. Statistical significance was defined as P < 0.05. Statistical analysis was performed with GraphPad 7.0b for Mac.

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 Table S1. Primer sequences for qRT-PCR.

Primer	Forward	Reverse			
RPL37A	GTGGTTCCTGCATGAAGACAGTG	TTCTGATGGCGGACTTTACCG			
MESP1	GTGCTGGCTCTGTTGGAGA	CAGAGACGGCGTCAGTTGT			
TBX5	GGGCAGTGATGACATGGAG	GCTGCTGAAAGGACTGTGGT			
ISL1	AAAGTTACCAGCCACCTTGGA	ATTAGAGCCCGGTCCTCCTT			
NKX2.5	CAAGTGTGCGTCTGCCTTT	TTGTCCGCCTCTGTCTTCTC			
TNNT2	AGCATCTATAACTTGGAGGCAGAG	TGGAGACTTTCTGGTTATCGTTG			
ETV2	CAGCTCTCACCGTTTGCTC	AGGAACTGCCACAGCTGAAT			
KDR	CCATCTCAATGTGGTCAACCTTCT	TCCTCAGGTAAGTGGACAGGTTTC			
VEC	GGCATCATCAAGCCCATGAA	TCATGTATCGGAGGTCGATGGT			
CD31	GCATCGTGGTCAACATAACAGAA	GATGGAGCAGGACAGGTTCAG			
MEOX2	CCAAGGATGCACAGTCTGG	AGGAGGAAAACCTTCGTGCTG			
GATA4	GACAATCTGGTTAGGGGAAGC	GAGAGATGCAGTGTGCTCGT			
GATA6	TCCAACTTCCACCTCTTCTAAC	TCTCCCGCACCAGTCATC			
MYL2	TACGTTCGGGAAATGCTGAC	TTCTCCGTGGGTGATGATG			
MYL7	CCGTCTTCCTCACGCTCTT	TGAACTCATCCTTGTTCACCAC			
MYL4	AAGCCTTTGTCAAGCACATCA	AGGACTCCATCTCAGCTCACC			
MYL3	AAGGAGGTCGAGTTTGATGCT	TCCTTGAACTCTTCAATCTGCTC			
MYH6	CCAGGTCAACAAGCTTCGAG	TGTCACTCCTCATCGTGCAT			
MYH7	AGTCCCAGGTCAACAAGCTG	GGGCTGAGCAGATCAAGATG			
TNNI1	GTGGGTGACTGGAGGAAGAA	GTGAGCTGGGTTGGAGAAGA			
TNNI3	CACCTCAAGCAGGTGAAGAAG	CAGGAAGGCTCAGCTCTCAA			
ACTN2	GATGGAGCACATTCGTGTTG	TGATCCATCAGGCCATTCTT			
TCAP	GGCAGAATGGAAGGATCTGAC	TGTCTCTGGGTGTCCTCCTC			
SCN5A	GAGCTCTGTCACGATTTGAGG	GAAGATGAGGCAGACGAGGA			
CACNA1C	CAATCTCCGAAGAGGGGTTT	TCGCTTCAGACATTCCAGGT			
KCNQ1	TCCTGGTCTGCCTCATCTTC	AAGAACACCACCAGCACGAT			
KCNE1	TCTCTGGCCAGTTTCACACA	CTCAAACTTCCCAGGCACAC			
KCNJ12	TGGATCCTTTCCAGTTGGTG	CGGCTCCTCTTGAGTTCTATCTT			
KCNJ2	CGCTTTTTACAAACCACTGGA	TGGGAGCCTTGTGGTTCTAC			
HCN4	CAATGAGGTGCTGGAGGAGT	GGTCGTGCTGGACTTTGTG			
NCX1	ACATCTGGAGCTCGAGGAAA	CTGGAATTCGAGCTCTCCAC			
SERCA2A	ACAATGGCGCTCTCTGTTCT	ATCCTCAGCAAGGACTGGTTT			
PLN	TCCCATAAACTGGGTGACAGA	TGATACCAGCAGGACAGGAAG			
RYR2	GCTATTCTGCACACGGTCATT	ATTTCCGTGCCACTTCCTTT			
CASQ2	CCGGGACAATACTGACAACC	CTTCTCCCAGTAGGCAACGA			
S100A1	CTGAGCAAGAAGGAGCTGAAAG	ACCTTGTCCACAGCATCCAC			

TRDN	GTGTCTCCCACAAAGCAGAAA	GGTCTGCAGGAGTGAAAGGA
NPPA	TGATCGATCTGCCCTCCTAA	TCCTCCCTGGCTGTTATCTTC
NPPB	GCTTTGGGAGGAAGATGGAC	TGTGGAATCAGAAGCAGGTGT
ACTA1	AAGAGCTACGAGCTGCCAGA	ACAGGTCCTTCCTGATGTCG
CKMT2	CAAGGACCCACGCTTTTCTA	TCCACCAGGTAATTGACTCCA
ITGA7	CATCCTCCTGGCTGTACTGG	GGAATCTTCACCGCATGGTA
COUPTFII	GCTTTCCACATGGGCTACAT	CAAGTGGAGAAGCTCAAGGC
FOXC2	GAGCCGTCTCGGAAGCAG	CCGCAGCCCGGTAGTAATTC
NRP1	AACACCAACCCCACAGATG	AAGTTGCAGGCTTGATTCG
NRP2	CTGGAAGCAGCATTGTGTG	TAACTCGCTGATGGGGAGA
HEY2	TCATGAAGTCCATGGCAAGA	TTGTGCCAACTGCTTTTGAA
NFATC1	GCCCCTATTCCTGTAACGGT	ATGTGGCAACTAGGAGTGGG
CX40	AATCAGTGCCTGGAGAATGG	CGAACCTGGATGAAACCTTC
β₁AR	AAGAGAAAGGATGGAGGCAAA	GCCCTACACAAGGAAAGCAA
β ₂ AR	TGGTGATCATGGTCTTCGTCT	TCCACCTGGCTAAGGTTCTG

 Table S2.
 Antibodies used for FACS and immunofluorescence analyses.

	Antibody	Company	Catalogue number	Dilution
	Anti-VCAM1-PE	R&D	FAB5649P	1:20
	Anti-CD34-APC	Miltenyi Biotech	130-090-954	1:20
FACS	Anti-KDR-PE	R&D	FAB357P	1:20
	Anti-VEC-PECY7	eBioscience	25-1449-42	1:100
	Anti-CXCR4-PE	BD Pharmigen	555974	1:20
	Anti-CD31-APC	eBioscience	17-0319-42	1:100
	Mouse IgG2a-APC	Miltenyi Biotech	130-098-850	1:20
	Mouse IgG2A PE	R&D	IC003P	1:20
	Mouse IgG1 PE	R&D	IC002P	1:20
	Mouse IgG1 K APC	eBioscience	17-4714-41	1:100
	TNNI	Santa Cruz	Sc-15368	1:500
	α-ACTININ	Sigma-Aldrich	A7811	1:800
Immunofluorescence	CD31	Dako	M0823	1:200
	СуЗ	Dianova	715-165-150	1:100
	AF488	Invitrogen	A21206	1:200

Study	Cardiac	Number of	CM source	EC source	CM culture medium	EC culture medium	Cardiac tissue	Substrate/scaffold	Assays performed	Purpose of the
	tissue given	cells per					medium (in the			study
	name	cardiac tissue					presence of ECs)			
Narmoneva et	Three-	0.7 x 10 ⁶	Neonatal	Mouse ECs	DMEM + 7% fetal calf	DMEM + 20% fetal calf	DMEM + 10% fetal	1% peptide	Immunofluorescence; cell	Transplantation
al., 2004	Dimensional	cells/cm2	mouse CMs	from heart and	serum	serum + porcine heparin	calf serum	hydrogel scaffolds	death assay;	
	culture	(CMs alone) or	(1-2 days	lungs		+ endothelial cell growth			evaluation of contractile	
		1.4 x 10 ⁶	old)	(6-8 weeks		stimulant			areas	
		cells/cm2		old)						
		(coculture)								
Caspi et al.,	Engineered	4 x 10 ⁵ cells	hESCs	hESCs or	Knockout DMEM + 20%	hESC-ECs: Endothelial	50% EGM-2 and 50%	Porous sponges	Immunofluorescence; cell	Transplantation
2007	cardiac	per tissue		HUVEC	fetal bovine serum	cell growth medium	standard ES cell	composed of 50%	viability assay; laser	
	tissue						culture medium	poly-L-lactic acid	scanning confocal Ca ²⁺	
						HUVEC: EGM-2 medium		(PLLA) and 50%	imaging	
						+ 2% FBS		polylactic-glycolic		
								acid (PLGA);		
								Matrigel		
Stevens et al.,	Cardiac	3 x 10 ⁶ cells	hESCs	hESCs or	RPMI + B27	hESC-ECs: huEB	huEB medium or	X	Immunofluorescence;	Transplantation
2009	tissue	per patch		HUVEC		medium (80% KO-DMEM	huEB medium +		Passive mechanical	
	patch					+ 20% FBS) + VEGF g	M199 medium or		measurements; in vivo	
						50 ng/mL	RPMI-B27 medium		transplantation into skeletal	
									muscle; engraftment in heart	
						HUVEC: EGM-2 medium				
Tulloch et al.,	Engineered	2 x 10 ⁶ CMs or	hESCs or	HUVEC	RPMI + B27 followed by	EBM2	80% Knockout-	Collagen type I,	Immunofluorescence;	Transplantation
2011	Myocardium/	2 x 10 ⁶ CMs	hiPSCs		80% Knockout-DMEM +		DMEM and 20% fetal	11% mouse	transmission electron	
	cardiac	+ 1 x 10 ⁶			20% fetal bovine serum		bovine serum	basement	microscopy; gene	
	muscle	HUVEC						membrane extract	expression profile; cardiac	
									engraftment	
Ravenscroft et	Cardiac	500 cells per	hESCs or	Primary	hESC-CM: RPMI + B27	Endothelial basal	50% RPMI + B27 (or	Х	Immunofluorescence; gene	Drug toxicity tests
al., 2016	Microtissue	100 μΙ	hiPSCs	human		medium MV2 + 5% FCS	iCell CM medium) +		expression profile; video-	
				coronary	hiPSC-CM: iCell CM	+ supplements(EGF,	50% MV2 medium +		based edge detection of	
				artery	maintenance media	bFGF, IGF, VEGF,	supplements		contraction; Ca ²⁺ transient	
				endothelial		Ascorbic Acid,			measurements	
				cells (HCAEC)		Hydrocortisone)				

Masumoto et	Engineered	3 x 10 ⁶ cells	hiPSCs	hiPSCs	RPMI+ B27	RPMI+ B27 + VEGF	High glucose-	Acid-soluble rat-tail	Contractile force	Transplantation
al., 2016	cardiac	per tissue					modified Dulbecco's	collagen type I	measurements; implantation	
	tissue						essential medium +	neutralized with	in rats; next-generation RNA	
							20% fetal bovine	alkali	sequencing	
							serum	Buffer;		
								Matrigel		
Mannhardt et	Engineered	1 x 10 ⁶ cells	hiPSCs	X	DMEM/F-12 followed by	X	DMEM + 10% horse	Agarose and	Contraction analysis	Transplantation
al., 2016	heart tissue	per tissue			RPMI		serum + 10 µg/ml	custom-made		
							insulin + 33 µg/ml	Teflon spacers		
							aprotinin	casting molds with		
								solid silicone racks;		
							(No endothelial cells)	Matrigel		
Huebsch et	Micro-Heart	2 x 10 ³ cells	hiPSCs	X	RPMI+ B27	X	Knockout Dulbecco's	PDMS stencils	Immunofluorescence;	Drug response
al., 2016	muscle	per tissue (+ 2					Modified Eagle		Scanning Electron	analysis
		x 10 ³ stromal					Medium + 20% fetal		Microscopy; Video	
		cells)					bovine serum		Microscopy based drug	
							following RPMI+ B27		response studies	
							medium			
Present study	Cardiac	5 x 10 ³ cells	hESCs or	hESC or	BPEL	BPEL + VEGF	BPEL + VEGF	X	Immunofluorescence; in	Cardiac disease
	microtissue	per tissue	hiPSCs	hiPSC					depth gene expression	modeling
		(5000 cells per							profile; MEA analysis;	
		50 µl)							contraction analysis	Drug screening
										Drug discovery

TABLE S3. Comparison between existing cardiac tissue models.

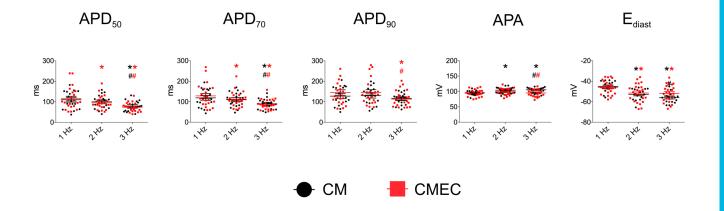


FIGURE S1

Figure S1. Rate dependency of cardiomyocytes differentiated upon CM and CMEC condition. Electrophysiological analysis of day 21 $NKX2-5^{eGFP/w}$ hESC cardiomyocytes differentiated under CM (black) and CMEC (red) conditions. * = p < 0.05 vs. 1 Hz. # = p < 0.05 vs. 2 Hz. Data were analyzed with repeated measurement. Two-way ANOVA with Sidak's multiple comparisons test. N = 16-24 from three independent differentiation experiments.

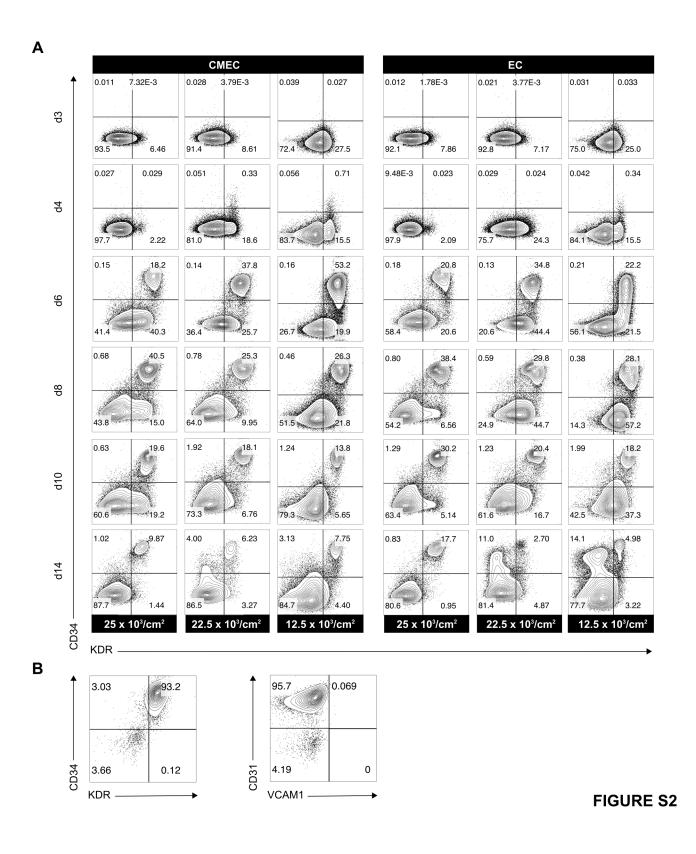


Figure S2. Isolation of CD34⁺ **endothelial cells.** (A) FACS plots for CD34 together with KDR of CMEC and EC populations measured in the NKX2.5^{eGFP/w} hESCs at the indicated time points (d=days) of differentiation at different cell-seeding densities. Numbers in the quadrants represent the respective percentage of cells. N = 1. (B) FACS plots for CD34 together with KDR (left panel) and for CD31 together with VCAM1 (right panel) of enriched CD34⁺ endothelial cells measured in the NKX2.5^{eGFP/w} hESCs after cryopreservation and replating. Numbers in the quadrants represent the respective percentage of cells. N = 1.

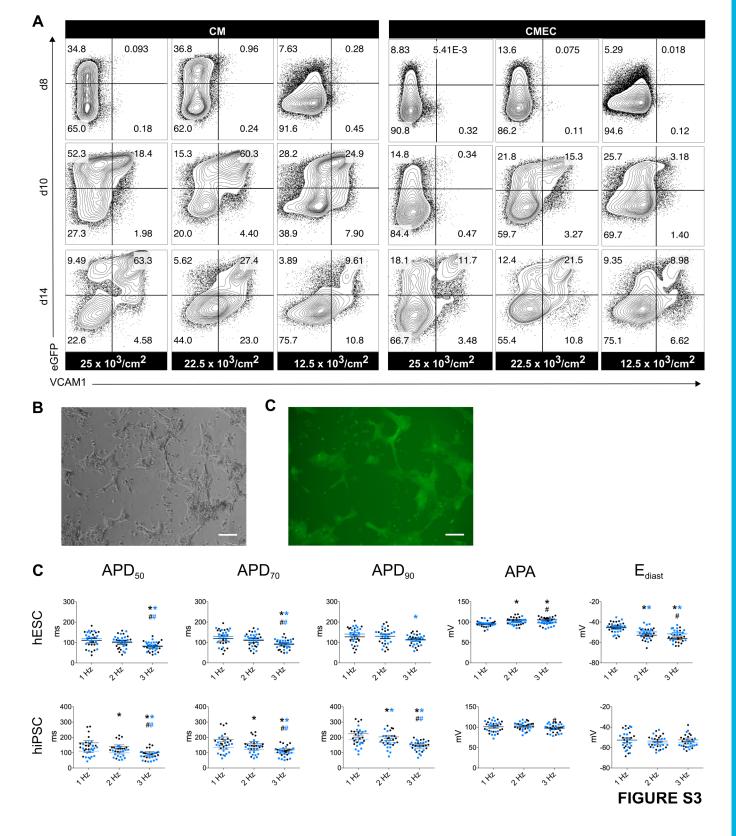
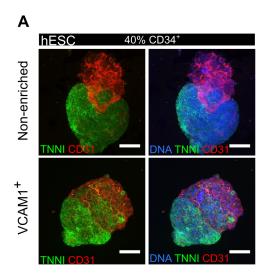


Figure S3. Isolation of VCAM1⁺ **cardiomyocytes.** (A) FACS plots for VCAM1 together with eGFP of CM and CMEC populations measured in the NKX2.5^{eGFP/w} hESCs at the indicated time points (d=days) of differentiation at different cell-seeding densities. Numbers in the quadrants represent the respective percentage of cells. N = 1. (B) Representative bright field and (C) GFP fluorescence images of the morphological appearance of CM-derived VCAM1⁺ cardiomyocytes from NKX2.5^{eGFP/w} hESCs after isolation and re-plating. Scale bar: 100 μm. (D) Rate dependency of non-enriched (black) and enriched VCAM1⁺ (blue) cardiomyocytes. Action potential parameters from cardiomyocytes differentiated from *NKX2-5*^{eGFP/w} and hiPSCs. * = p < 0.05 vs. 1 Hz. # = p < 0.05 vs. 2 Hz. Data were analyzed with repeated measurement Two-way ANOVA with Sidak's multiple comparisons test. N = 16-16 for hESCs and N=15-18 for hiPSCs, each from three independent differentiation experiments.



B hESC

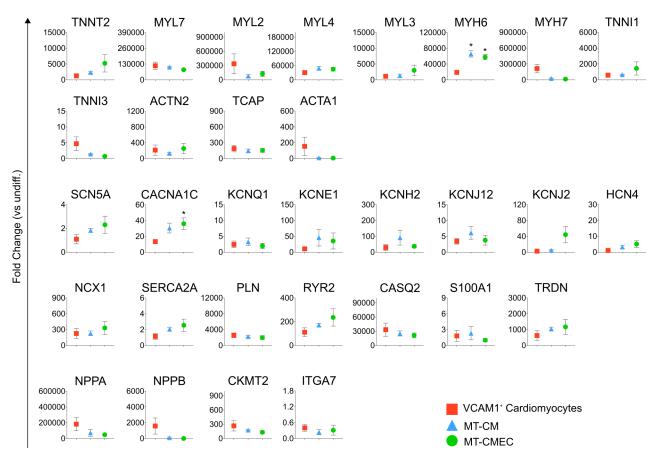


FIGURE S4

Figure S4. Characterization of day 7-MTs from hESCs. (A) Immunofluorescence analysis of sarcomeric cardiomyocyte TNNI (green) and endothelial cell surface marker CD31 (red) of cardiac MTs from non-enriched (upper panel) and enriched VCAM1⁺ (lower panel) cardiomyocytes. Immunofluorescence data refer to day 7-MTs generated from *NKX2-5*^{eGFP/w} hESCs. Percentages of CD34⁺ cells are shown at the top. Nuclei are stained in blue with DAPI. Scale bar: 100 μm. (B) qRT-PCR analysis for key sarcomeric genes, ion channels and calcium-handling genes, as well as other cardiac genes of interest on day 7 MT-CM, MT-CMEC and on day 21-age-matched VCAM1⁺ cardiomyocytes from hESCs. All values are normalized to *RPL37A* and are relative to undifferentiated hESCs. Ordinary one-way ANOVA with Tukey's multiple comparisons test. * = P < 0.05 vs. VCAM1⁺ cardiomyocytes. N ≥ 3. Data are shown as mean ± SEM.

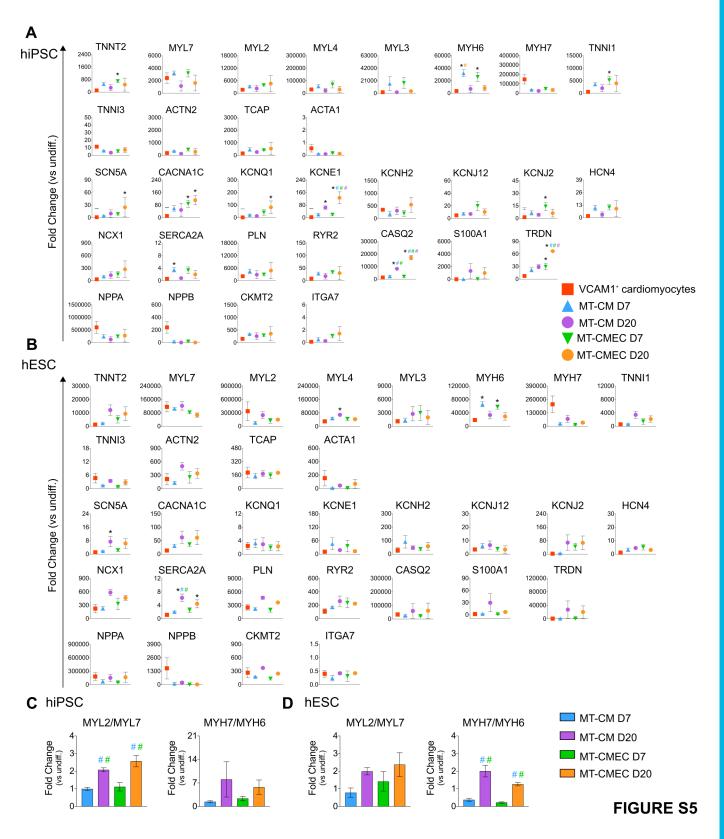


Figure S5. Gene expression profile of day 20-MTs. (A) qRT-PCR analysis for key sarcomeric genes, ion channels involved in AP shaping and calcium regulatory genes, as well as other cardiac genes of interest on day 7 and day 20 MT-CM and MT-CMEC together with VCAM1 $^+$ cardiomyocytes generated from hiPSCs and (B) hESCs. All values are normalized to *RPL37A* and are relative to undifferentiated hiPSCs or hESCs. Ordinary one-way ANOVA with Tukey's multiple comparisons test. * = P < 0.05 vs. VCAM1 $^+$ cardiomyocytes. # = P < 0.05 vs. corresponding colour coding group. N \ge 2. Data are shown as mean \pm SEM. (C) qRT-PCR analysis for *MYL2/MYL7* ratio (left panel) and *MYH7/MYH6* ratio (right panel) on day 7 and day 20 MT-CM from hiPSCs and (D) hESCs. Values are normalized to *RPL37A* and relative to undifferentiated hiPSCs or hESCs. Ordinary one-way ANOVA with Tukey's multiple comparisons test. # = P < 0.05 vs. corresponding colour coding group. N \ge 2. Data are show as mean \pm SEM.

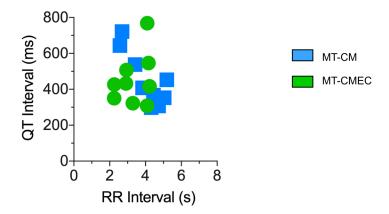


FIGURE S6

Figure S6. Rate-dependency of MTs by MEA. Correlation between QT-interval and RR-interval from MT-CM (blue) and MT-CMEC (green) from hiPSCs. A comparable electrical phenotype was exhibited by both MT-CM and MT-CMEC, indicating that the presence of endothelial cells did not affect the QT-RR relationship.

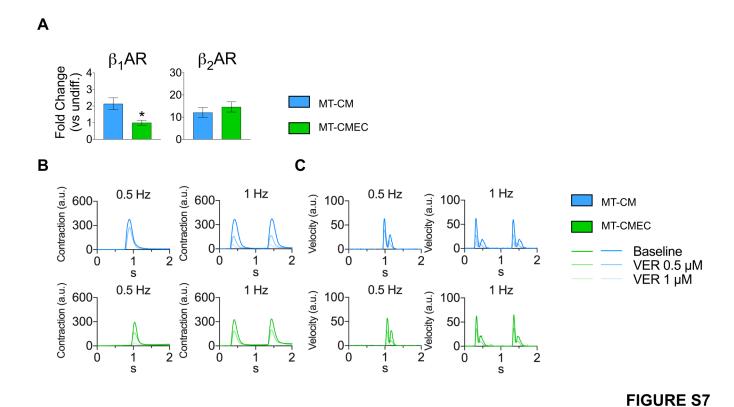
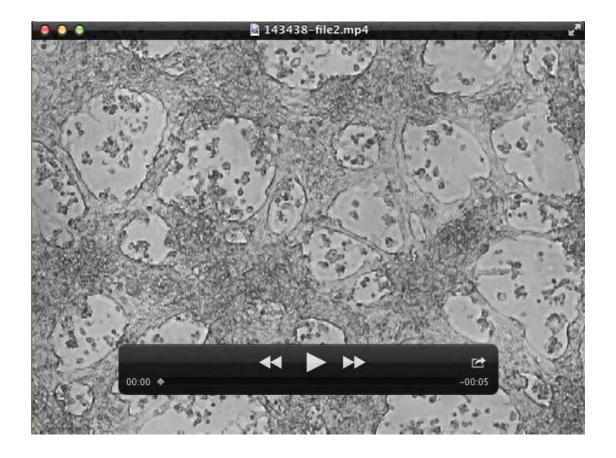


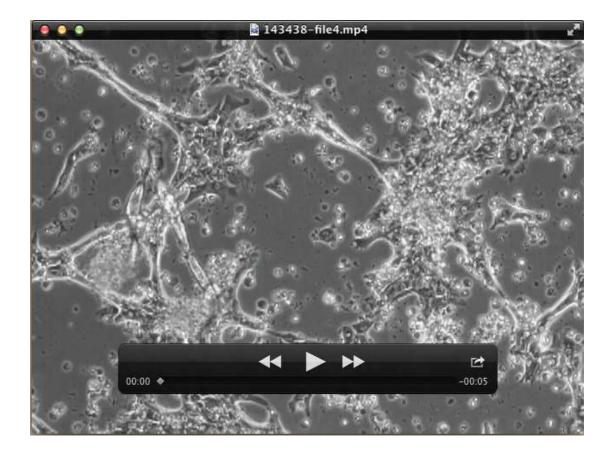
Figure S7. β-adrenoreceptors and contraction profile of MTs from hESCs. (A) qRT-PCR analysis of β-adrenoreceptors ($β_1$ AR, left panel; $β_2$ AR, right panel) in day-7 MT-CM and MT-CMEC from hESCs. Values are normalized to *RPL37A* and relative to undifferentiated hESCs. Mann-Whitney test. * = P < 0.05 vs. MT-CM. N = 3. Data are show as mean ± SEM (B) Representative traces of contraction and contraction velocity (C) profiles of MT-CM (blue) and MT-CMEC (green) generated from hESCs and paced at 0.5 and 1 Hz, in baseline and after superfusion of 500 nM and 1 μM VER.



 $\label{eq:Movie 1} \textbf{Movie 1}$ Beating monolayers of day 10-differentiated NKX2.5 $^{\text{eGFP/w}}$ hESCs upon CM condition.



Movie 2Beating monolayers of day 10-differentiated NKX2.5^{eGFP/w} hESCs upon CMEC condition.



Movie 3Beating monolayers of hiPSC-VCAM1+ cardiomyocytes after isolation and re-plating.